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Mas-Cabo, J.; Prats-Boluda, G.; Perales Marín, AJ.; Garcia-Casado, J.; Alberola Rubio, J.; Ye Lin, Y. (2019). Uterine electromyography for discrimination of labor imminence in women with threatened preterm labor under tocolytic treatment. *Medical & Biological Engineering & Computing*. 57:401-411. <https://doi.org/10.1007/s11517-018-1888-y>



The final publication is available at

<http://doi.org/10.1007/s11517-018-1888-y>

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Additional Information

1 **TITLE PAGE**

2 **Journal:**

3 Medical & Biological Engineering & Computing

4 **Title of paper:**

5 Uterine electromyography for discrimination of labor imminence in women with threatened preterm
6 labor under tocolytic treatment

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18 **Total number of words in the manuscript:** 5731

19 **Number of words of the Abstract:** 195

20 **Number of Figures:** 6

21 **Number of Tables:** 3

22

23 ABSTRACT

24 Current techniques used in clinical practice present serious limitations to detect imminent delivery in patients
25 with threatened preterm labor being this an outstanding goal in obstetrics. Electrohysterogram (EHG) has
26 emerged as an alternative technique, providing relevant information about labor onset when recorded in
27 controlled checkups without tocolytic drugs. Those works are mainly focused on EHG-bursts analysis and to a
28 lesser extent whole EHG windows analysis. No studies have compared the performance of both methods for
29 labor prediction using the same database. We assessed the capability of EHG signals to discriminate the
30 imminence (< 7 days) of labor in women with threatened preterm labor under tocolytic therapy, using both
31 EHG-burst and whole EHG window analyses, by working out temporal, spectral and non-linear parameters.
32 Only non-linear parameters distinguished those women who delivered in less than 7 days from the rest, for
33 both EHG-burst (2 parameters) and whole EHG window analysis (4 parameters). Therefore, EHG provides
34 relevant information about labor imminence even being recorded in women with threatened preterm labor
35 under tocolytic therapy. Indeed, whole EHG window outperforms EHG-burst analysis promoting the
36 development of real-time systems to predict imminent labor approaching the use of EHG in clinical praxis.

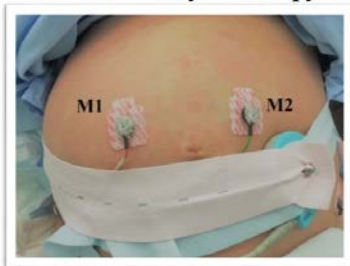
37 **Keywords:** Electrohysterogram, premature labor, tocolytic therapy, non-linear analysis.

38

39 GRAPHICAL ABSTRACT

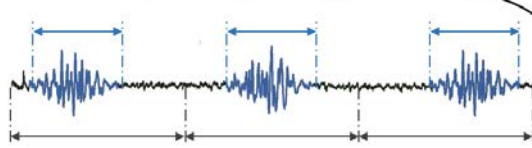
40 The capability, for imminent labor prediction (labor <7 days), of EHG recordings carried out on preterm
41 threatened patients and under tocolytic therapies is analyzed by using EHG-burst and whole EHG window
42 analysis. Compared to temporal and spectral parameters, non-linear features had a better performance in the
43 separation of women who delivered in less or more than 7 days

*Women with threatened preterm labor
& under tocolytic therapy*



Imminent Labor?

○ EHG-Burst Analysis



● Whole EHG window Analysis

Non-linear Characterization



G1: Labor <7 & G5: Labor >7

44

45

46 1. INTRODUCTION

47 Premature births are defined as childbirths occurring prior to week 37 of gestation and constitute a leading
48 cause of neonatal mortality and morbidity, cognitive impairments, cardiovascular system complications and
49 up to 40% of these survivors develop chronic lung disease [12, 26]. In developed countries, preterm birth
50 rates, the major cause of mortality excluding congenital malformations [18], are about 12% of total births [12]
51 and seem to be on the rise [11]. These situations entail a high cost for families and the health systems. Studies
52 carried out in US have found that preterm births costs can be five times higher than those of term labor ones
53 [26].

54 Different methods are traditionally used to diagnose preterm labor, some based on the measurement of the
55 cervical length, dilatation and consistence of the cervix, such as the Bishop score [8]. However, all these
56 techniques are limited when it comes to predicting preterm labor [8, 20]. A better method of diagnosing
57 imminent labor is thus needed for women with threatened preterm labor (TPL) to minimize unnecessary
58 hospitalizations, reduce healthcare costs and improve maternal and fetal well-being [4].

59 Uterine contractility is monitored during pregnancy to evaluate the threat of preterm labor. The most common
60 technique for evaluating uterine contractility is by external tocodynamometry (TOCO) [13]. Nevertheless,
61 TOCO presents some disadvantages and limitations such as the required re-positioning, its effectiveness
62 depends on the subjectivity of the clinician and it do not provide any information on the efficiency of uterine
63 contractions, which is essential information for detecting true preterm labor [16]. An alternative method of
64 monitoring and analyzing uterine contractility is by external measurement of the uterine electrical activity
65 [13]. This technique, also called electrohysterography (EHG), records non-invasively the electrical activity
66 associated with the contraction of the myometrial cells of the uterus (EHG-bursts) [9, 13]. Literature report
67 that EHG characteristics are ‘dynamic’, and they change throughout pregnancy [3, 5]. At early gestational
68 ages the uterine electrical activity is scarce and poorly coordinated, however as labor approaches it becomes
69 more and more intense and synchronized [5, 9]. Several studies have focused on using EHG parameters to
70 identify ‘true’ labor contractions and ‘false’ labor contractions in term and preterm pregnancies from EHG
71 recordings carried out in routine checkups, without any drug being administered to women [6, 24, 28, 29].
72 However, the applicability of this technique in clinical practice still remains unclear, since tocolytic agents are

73 usually given at the first signs of threatened preterm labor, impairing uterine myoelectrical activity. Few
74 studies have conducted on women with threatened preterm labor under tocolytic agents [28], thus not having
75 analyzed EHG parameters (linear and non-linear) capability to predict labor horizon under this common
76 clinical situation. Furthermore, factors that could limit the clinical application of EHG technique include the
77 entangled acquisition systems ordinary used in the research field, whose use is not viable in clinical practice,
78 and the need for identification of EHG-bursts, which is in contrast to the need of simplified protocols and
79 automated segmentation processes in clinical environments. In this regard, almost all the studies in this field
80 focus on the analysis of EHG-bursts [10, 21, 24]. The segmentation of EHG-burst is a process that depends on
81 the experts' subjectivity and requires a long time [6], making this analysis unsuitable for real time diagnostic
82 systems. Some authors propose whole EHG window analysis [7], which greatly simplifies the segmentation
83 process and could make EHG analysis suitable for real time applications and so more attractive to clinicians.
84 Even if the above-mentioned types of analysis have been reported by several authors in the literature, there is
85 no work extant that compares the imminent labor prediction capacity of both methods.
86 Therefore, with the purpose of bringing closer the use of EHG to clinical praxis, the aim of the present work is
87 to study the feasibility of EHG parameters (linear and non-linear) to discriminate, whether delivery will occur
88 in more or less than 7 days from the EHG recording, in women with threatened preterm labor, under different
89 stages of tocolytic treatment and using a simplified EHG recording system. The results provided by
90 conventional EHG-burst analysis will be compared with those from whole EHG window analysis.

91 2. MATERIALS & METHODS

92 2.1. DATA ACQUISITION

93 Eighty eight EHG recording sessions with a duration between 30 and 60 minutes conducted on 51 patients
94 with singleton pregnancies are included in this study. All the recordings were carried out at the "Hospital
95 Universitario y Politécnico La Fe", in Valencia, whose Institutional Review Board approved this study, which
96 adheres to the Declaration of Helsinki. All patients were informed about the nature of the study and the
97 recording protocol and signed a written informed consent form. Women included were in gestational ages
98 between 25 and 36 weeks and showing symptoms of preterm labor, such as cervical effacement or regular

99 uterine dynamics. These situations entailed that most of the records (91 %) were carried out under the effect of
100 tocolytic drugs.

101 The patients enrolled in the study were followed up until their labor ended, and those who presented risk of
102 preterm labor but finally did not initiate labor spontaneously were excluded. The following obstetric data was
103 collected: gestational age, previous gestations, abortions, parity, cervical length and if the EHG recording was
104 performed without, during or after tocolytic treatment. Table 1 shows the obstetric data of the subjects
105 involved in the study. Furthermore additional information about the Database obstetrical information is shown
106 in Figure 1 in form of histograms.

107 *Insert Table 1*

108 *Insert Figure 1*

109 In order to study the capability to discriminate labor in less than 7 days in threatened preterm women under
110 tocolytic treatment, the evolution of different EHG parameters as labor approaches was analyzed. Thus the
111 recordings were divided into four groups, according to their time to delivery (TTD). G1 includes women who
112 gave birth in less than 7 days after the recording session, G2 is composed of recordings from women who
113 gave birth between 7 and 14 days after the recording session, and G3 and G4 are formed by recordings from
114 women who delivered between 14 to 30 days, and more than 30 days, respectively. In order to study the utility
115 of EHG parameters in distinguishing between patients who gave birth in less than or more than 7 days, an
116 extra group G5 was considered, formed by all the patients who delivered in more than 7 days (G2 + G3 + G4)
117 after the recording. Figure 2 graphically represents the distribution of all the registers included in the different
118 groups and the time to delivery associated with each group.

119 *Insert Figure 2*

120 For each recording session, the abdominal surface was prepared to reduce skin-electrode impedance by an
121 abrasive paste (Nuprep, Weaver and Company, USA). The EHG signal was registered by placing two
122 disposable monopolar Ag/AgCl electrodes (3M red dot 2560, USA) symmetrically with respect to the median
123 axis on the supraumbilical zone, the inter-electrode distance being 8 cm. Another two disposable electrodes

124 were placed on each hip as reference and ground electrodes. This configuration was chosen to simplify the
125 acquisition protocol, allowing simultaneous clinical recordings with other medical devices, such as TOCO and
126 ultrasounds. Figure 3 shows the configuration of the disposable electrodes together with TOCO and
127 ultrasound for fetal heart rate monitoring.

128 The signals picked up by the electrodes were conditioned by two custom-made amplifiers, which provide a
129 2059 V/V gain in the band 0.1 to 150 Hz. After amplification, the signals were digitalized with a 24 bit ADC
130 at 500 Hz. Further information on this wireless signal recording module, developed ad hoc by this group can
131 be found in the original paper [33]. From these two monopolar electrodes, a bipolar signal was obtained as the
132 difference between M1 and M2, where M1 and M2 are the monopolar signals registered by the two disposable
133 electrodes. The TOCO signal was simultaneously acquired using a Corometrics 170 from (GE Medical
134 Systems, USA) and transmitted to the PC with a sampling frequency of 4 Hz.

135 *Insert Figure 3*

136 2.2. DATA ANALYSIS

137 EHG signals were digitally filtered in the range 0.1 to 4 Hz, since most of their spectral content distributes
138 mainly in that range [24], by a 5th order Butterworth bandpass digital filter. EHG signals were also resampled
139 at 20 Hz.

140 As previously mentioned, the present work tackles both classical EHG-burst and whole EHG window
141 analysis. EHG-burst were manually segmented by the following criteria: significant amplitude and frequency
142 changes regarding the basal tone with durations greater than 40 s, and absence of motion artefacts and
143 respiratory interference [28]. A total of 338 analyzable EHG-bursts were obtained. For the whole EHG
144 window analysis, only segments corresponding to patient motion artifacts or fetal movements were detected
145 by visual inspection and discarded (\approx 2824 minutes of analyzable EHG records). These segments were divided
146 into analysis windows of 120 s with 50% overlap, in order to include representative sections of the recording
147 at a reasonable computational cost. Preliminary studies were performed to determinate the optimal bandwidth
148 for the whole EHG window analysis working out parameters in window sizes of: 1, 2 5 and 10 min of
149 duration. Results were very similar for windows of 2, 5 and 10 min, selecting finally a size of 2 min in order
150 to reduce the computational cost.

151 Figure 4A includes a diagram of how EHG parameters were calculated for the EHG-burst analysis, and Figure
152 4B shows the procedure to obtain the same EHG parameters in the whole EHG window analysis.
153 For both analyses (EHG-burst and whole EHG window), a set of temporal, spectral (obtained from Welch
154 periodogram), and non-linear parameters (which measure time series complexity) were calculated (8 in total):
155 peak to peak amplitude of the EHG signals, median frequency, dominant frequency, sample entropy (length of
156 repeated templates: 2, tolerance: 0.15) [32], spectral entropy [35], time reversibility [15], multistate Lempel-
157 Ziv index [2, 35] (including 6 states) and binary Lempel-Ziv index [2, 35]. As for temporal and spectral
158 parameters, we computed others like RMS, median frequency, H/L ratio, deciles and Teager, which showed
159 similar results to those obtained from App, MF and DF [27]. Therefore, so as to be concise only results for the
160 last three parameters are shown in the present manuscript. Regarding non-linear parameters, sample and
161 spectral entropy measure the complexity of a finite time series in time and spectral domain respectively, and
162 they provide higher values for more “chaotic” signals [6, 32]. As for time reversibility estimates “how similar”
163 a time series looks like when viewed in forward or reverse time [15]. Lempel-Ziv indexes evaluate signal
164 complexity by counting the number of different patterns in a time series [2, 35]. Lempel-Ziv multistate
165 approach was included in order to evaluate high frequency and low amplitude signal components [2]. After
166 obtaining the EHG parameters from each EHG-burst and/or each analysis window, the median values of each
167 EHG parameters were worked out for every recording session.
168 For each parameter, a Wilcoxon ranked test ($\alpha = 0.05$) was performed in order to assess whether its median
169 values differ between different groups (G1, G2, G3, G4) and between G1 and G5 for both EHG-burst analysis
170 and whole EHG window analysis. Moreover, a post hoc power analysis of each parameter and analysis (EHG-
171 Burst and whole EHG window analysis) has been carried out to assess the clinical significance to differentiate
172 between G1 and G5.

173 *Insert Figure 4*

174 3. RESULTS

175 Figure 5 shows 1000 s of EHG bipolar records from women with threatened preterm labor from the four
176 groups considered: G1, G2, G3 and G4, which correspond to less than 7 days, 7 to 14 days, 14 to 30 and more
177 than 30 days from the EHG recording to delivery, respectively. Several high amplitude EHG-bursts (≈ 250 –

178 300 μV) can be easily identified in the EHG recording of the patient from G1. It can be noticed how EHG-
179 burst amplitude decreases as TTD increases: G2 ($\approx 170 \mu\text{V}$), G3 ($\approx 150 \mu\text{V}$) and G4 ($\approx 100 \mu\text{V}$).

180 *Insert Figure 5*

181 Tables 2 and 3 show the mean and standard deviation of the values of the parameters obtained from EHG
182 records for the EHG-burst analysis and the whole EHG window analysis are shown in respectively. For easier
183 visual analysis, in Figure 6 the median values of each parameter for both EHG-burst analysis and whole EHG
184 window analysis are displayed according to the time to delivery. It also shows the significant differences
185 obtained between the different groups for both analyses performed, represented by black and white dots in the
186 upper part of each graph. If there is any significant difference between patients who delivered in less than 7
187 days (G1) and those who delivered in more (G5) it is also indicated in the lower part of them (blue braces).

188 *Insert Table 2*

189 *Insert Table 3*

190 *Insert Figure 6*

191 Regarding temporal and spectral parameters, an increase in the amplitude values (A_{pp}) as labor approaches
192 can be observed in Figure 6, being more evident in EHG-burst analysis than in whole EHG window analysis.
193 Despite this, significant differences were only obtained for G3 vs. G4 ($p: 0.028$, EHG-burst analysis and $p:$
194 0.027 , whole EHG window analysis). No clear tendency is exhibited for median frequency (MF) (see Figure
195 6) for either EHG-burst or whole window analysis. For this parameter significant differences were only
196 obtained when comparing G3 vs. G4 for whole EHG window analysis. The dominant frequency (DF)
197 exhibited a decreasing trend from G4 to G1 in EHG-burst analysis (G1: $0.349 \pm 0.03 \text{ Hz}$, G4: $0.366 \pm 0.04 \text{ Hz}$,
198 Table 2) whereas in the whole EHG window analysis it barely changes (see Figure 6). However, no significant
199 differences were found between women who delivered in less than seven days and those who gave birth in
200 more than seven for both whole EHG window analysis and EHG-burst analysis.

201 Regarding the non-linear parameters, as can be seen in Figure 6, sample entropy present almost no changes as
202 labor approaches, for both EHG-burst analysis and whole EHG window analysis and in none of the performed
203 analyses shows significant differences between groups G1 and G5. By contrast, spectral entropy decreased
204 remarkably and in the case of the whole EHG window analysis it presents a notable ability to distinguish
205 between different groups (G1 vs. G4 ($p = 0.001$), G2 vs. G4 ($p = 0.015$), G3 vs. G4 ($p = 0.039$) and G1 vs. G5

206 ($p = 0.009$). This parameter presents a post hoc power of 93.2% when differentiating between G1 vs G5.
207 These are encouraging results since the spectral entropy has not been used previously to characterize EHG
208 changes along gestation, and it could provide useful information about labor onset under whole EHG window
209 analysis.

210 On the other hand in Figure 6, time reversibility seems to increase, for the whole EHG window analysis, in
211 groups close to labor, compared to those further from delivery. For the whole EHG window analysis
212 significant differences were found when comparing G1 and G5 ($p = 0.037$). However, this parameter
213 presented a post hoc power of 5.4%, probably due to the high variability in its values. Finally, regardless of
214 the status number (binary or multistate), Lempel-Ziv indexes present a similar trend to sample and spectral
215 entropy, decreasing as labor approaches for both EHG-burst and whole EHG window analysis. The results
216 obtained when comparing different groups are very similar in the two analyses, and statistically significant
217 differences were obtained for both when comparing G1 vs. G4, G2 vs. G4, G3 vs. G4 and G1 vs. G5. Lz-Bin
218 and Lz-Multi exhibited a post hoc power up to 90% for both analysis when differentiating G1 and G5.

219 In short, despite the fact that amplitude and spectral parameters present changing trends throughout gestation,
220 they do not discriminate well between the groups for both EHG-burst and whole EHG window analysis.
221 Furthermore, neither signal amplitude nor spectral parameter shows a statistically significant difference
222 between G1 and G5. On the other hand, a remarkable trend can be observed for non-linear parameters when
223 labor approaches (except for SampEntr), especially when applying the whole EHG window analysis. In order
224 to discriminate threatened preterm women who delivered in less than 7 days from those who gave birth in
225 more, statistically significant differences were found in 2 and 4 non-linear parameters for EHG-burst analysis
226 (LZ-Bin and LZ-Multi) and whole EHG window analysis (SpEntr, Time Rev, LZ-Bin and LZ-Multi),
227 respectively. Nevertheless post hoc power analysis indicated that Lz-Bin and Lz-Multi are able to discriminate
228 between G1 and G5 groups in both EHG-Bursts and whole EHG Windows analysis and SpEntr when
229 computed in whole EHG window analysis.

230 4. DISCUSSION

231 Imminent labor prediction in women with threatened preterm labor still remains as a major challenge in
232 clinical praxis. Electrohysterography has proven to provide more accurate information about labor onset

233 compared with the current clinical techniques. However, most studies were carried on woman far from labor
234 without the effect of tocolytic therapies –regular checkups- and usually with entangled and complex
235 acquisition protocols designed for research purposes. In this study, the capability for imminent labor
236 prediction of EHG records carried out in women with threatened preterm labor, under common clinical
237 conditions and using a simplified acquisition protocol was evaluated. EHG signals were mainly recorded in
238 women under tocolytic therapies (30) or after tocolytic treatment (51), only 7 women were recorded previous
239 tocolytics. This is because that EHG signals were recorded in threatened preterm women who were
240 hospitalized and not at the hospital emergency rooms. Although more than one recording session was obtained
241 from the same woman, only recordings corresponding to different situations (without, under and post tocolytic
242 therapy) have been included in this study.

243 As for EHG characterization, temporal, spectral and non-linear parameters computed from both EHG-burst
244 and whole EHG window analyses were worked out.

245 *4.1 EHG Temporal parameters as labor approaches*

246 Regarding temporal parameters, although our results showed an increase in both EHG-burst amplitude and
247 whole EHG window amplitude as labor approaches, a significant difference was only obtained for G3 vs. G4
248 (labor between 14-30 days' vs. labor for more than 30 days), and no significant differences were obtained
249 between patients who delivered in less than or more than 7 days, either in EHG-burst or whole EHG window
250 analysis. These results suggest that amplitude related parameters are not reliable indicators for determining the
251 proximity of delivery, which agrees with other authors who state that classical contraction parameters such as
252 duration, amplitude as well as RMS and intensity were not capable of differentiating between the preterm and
253 term delivery groups [17]. By contrast, other studies have found significant differences in RMS values
254 between deliveries in less than and more than 14 days for whole EHG window analysis [25]. These
255 differences could be mainly due to the different bandwidth used by the authors (1 – 1500 Hz) and may not be
256 attributable to EHG activity. They also computed the RMS value only for EHG-burst signals and also
257 considered a different time to delivery (TTD <14 vs TTD >14). Other factors related with the acquisition
258 protocol and skin preparation can also affect the amplitude values of the EHG signals, making this parameter
259 by itself unreliable for imminent labor prediction.

260 *4.2 EHG Spectral parameters as labor approaches*

261 Some authors highlight a shift of the spectral content towards high frequencies when delivery approaches [5,
262 28]. One of the most studied and useful uterine EMG measurements for predicting preterm labor is peak
263 frequency, which increases in women who deliver prematurely [20, 24]. Lemancewicz et al found that the
264 dominant frequency for whole EHG window analysis, estimated within the frequency range 0.24-4 Hz could
265 be used for differentiating patients who delivered within 7 days from those delivered after 7 days [19]. Other
266 studies suggest that median frequency could be used to discriminate term and preterm labors, for both whole
267 EHG window analysis [6] and the EHG-burst analysis [17]. Nevertheless, no statistically significant
268 differences were found in our results for either the frequency peak or mean frequency for distinguishing the
269 G1 vs. G5 group (labor in less than 7 days' vs. more than 7 days'). Indeed, for the EHG-burst analysis only
270 DF parameter showed significant differences when comparing G1 vs. G4 ($p = 0.049$), and in the whole EHG
271 window analysis only MF in comparing G3 vs. G4 ($p = 0.018$) and DF when comparing G1 vs. G3 ($p = 0.031$)
272 showed significant differences. These results could mainly be due to several factors. Firstly, previous studies
273 have shown that the shifting of the spectral content toward higher frequencies is produced 24 h before delivery
274 for term labors and 4 days before in preterm ones [22], and in our database, 7 of the 14 records included in the
275 group TTD <7 were between 4 to 7 days before delivery. Indeed, studies on the evolution of EHG spectral
276 parameters vs. TTD that use broad time horizons (several weeks before delivery) suggest their evolution is
277 clearly non-linear. Furthermore a shift to lower frequency content 10 days before delivery was found for
278 preterm patients [22] and other authors noted an increase of the signal energy in ranges [0.3 – 0.9] Hz and [1.2
279 – 1.5] Hz between 6-8.5 weeks before labor, then a decrease of about 4.5 to 5.5 weeks before labor and finally
280 a further increase 0.5 to 1 week before delivery for term labor patients [23]. Secondly, almost all EHG records
281 ($\approx 91\%$) included in the present work were taken from patients who received tocolytic treatment. We consider
282 that this real clinical condition could cause differences in the results when compared to other studies, since the
283 ability of tocolytic drugs such as Nifedipine has been shown to affect the amplitude and spectral content of the
284 EHG signals, resulting in smaller amplitude signals and in a significant decrease of PSD peak frequency [30].

285 *4.3 EHG Non-linear parameters as labor approaches*

286 With reference to SampEn, literature has reported controversial results: some authors state that SampEn
287 calculated in the range [0.3 - 3] Hz for whole EHG window analysis presented a downward trend when labor
288 is closer [6], other studies reported that for EHG-burst analysis no significant differences were obtained in
289 sample entropy between preterm and term records [17]. Vrhovc et al revealed that SampEn showed a non-
290 linear trend throughout pregnancy [31]. However, in the present work the SampEn did not show any
291 remarkable trend. These controversial results may be related with different factors such as differences in
292 recording protocols, analysis bandwidths or the inclusion criteria of the signal segments analyzed. In the
293 present work, we have discarded EHG segments with evidences of motion artifacts or respiratory interference
294 as they can affect non-linear parameters. Indeed SampEn has been proven to be sensitive to motion artifacts,
295 sampling frequency, the length of the embedded vectors (m) and the tolerance (r) [1, 6, 34].

296 As for Lempel-Ziv index, Lemancewicz found significantly higher values in the range [0.24 - 4] Hz for TTD
297 <7 days group against TTD >7 group [19]. Our results show that Lempel-Ziv in the range [0.1 - 4] Hz tend to
298 decrease as labor approaches for both EHG-burst and whole EHG window analysis, which indicates that the
299 EHG signal becomes more regular and deterministic. These differences with the Lemancewicz results may be
300 due to specific computing details, such as different bandwidth, and size of analysis window and/or others
301 related with inclusion or exclusion criteria of the EHG signals segments affected by motion artifacts or
302 respiratory interference. Moreover post hoc power analysis reveals that both LZ-Bin and LZ-Multi are robust
303 parameters to determine imminent labor regardless the type of analysis (EHG-Burst or whole EHG window
304 analysis) and therefore they could be potentially used for designing preterm labor prediction systems.

305 For the time reversibility parameter, other authors found that Time Rev increases as labor approaches in term
306 patients, reaching an AUC to distinguish labor contractions of 0.99 [15]. The same trends for both types of
307 analysis are observed in the present study, although significant differences for TTD <7 days group against
308 TTD >7 group were only obtained for whole EHG window analysis. However, our results reveals a high
309 variability in Tr values, which results in a low post hoc power value (5.4%). Then we consider that Tr is not a
310 robust parameter for predicting imminent labor in threatened preterm women under tocolytic therapies.

311 As far as we are concerned, the spectral entropy parameter has not been previously computed in EHG signals.
312 It has been previously used in the literature to evaluate the organization of the spectral content in EEG signals
313 picked up from patients during anesthesia [14]. In the present study, this parameter shows a downward trend

314 as labor approaches, giving rise to a very promising result, especially in whole EHG window analysis to
315 identify patients who give birth in less than 7 days.

316 *4.4 EHG-burst or whole EHG window analysis*

317 In general, whole EHG window outperforms EHG-burst analysis in terms of distinguishing (statically
318 significant differences of EHG parameters) recordings from different TTD groups. Specifically, the results for
319 whole EHG window analysis showed that all the tested non-linear parameters, except for SampEn, presented
320 statistically significant differences for women who delivered before 7 days and those after 7 days. In contrast,
321 when using EHG-burst analysis, only binary and multistate LZ parameters presented statistically significant
322 differences. Therefore, the use of complexity parameters in whole EHG window analysis in patients under
323 common clinical conditions could lead to a promising tool for predicting labor in less than 7 days. All these
324 results show that the whole EHG window analysis is not only able to track the evolution of EHG as labor
325 approaches, but it may have a better performance than EHG-burst analysis for predicting whether a patient
326 with threatened preterm labor will deliver in more or less than 7 days. These are remarkable results, since
327 whole EHG window analysis greatly simplifies the segmentation process as compared to traditional EHG-
328 burst analysis which is usually tedious, subjective and offline. In this regard, the use of an automatic classifier
329 able to discard patient motion artifacts, fetal movements and respiratory interference in combination with a
330 whole EHG window analysis system would facilitate the use of EHG techniques in clinical practice.

331 5. CONCLUSIONS

332 This paper analyzes the feasibility of the EHG to discriminate those patients with threatened preterm labor
333 who delivered in less than 7 days from those who delivered in more, under common clinical conditions, by
334 calculating linear and non-linear parameters computed from both EHG-bursts and whole EHG window
335 analyses. Although some temporal and spectral parameters showed an increasing trend as labor approaches in
336 both EHG-burst and whole EHG window analysis, complexity parameters presented a better performance in
337 distinguishing between the different time-to-delivery groups. For the EHG-burst analysis two non-linear
338 parameters (LZ-Bin and LZ-Multi) presented significant differences ($p < 0.05$) between groups of women who
339 delivered in <7 days vs. >7 days and four non-linear parameters for whole EHG window analysis (SpEntr,
340 Time Rev, LZ-Bin and LZ-Multi). It point out that whole EHG window analysis could be used to predict
341 preterm labor under common clinical conditions with better performance than the classical EHG-burst

342 analysis. Since this method does not require EHG burst annotation, this together with automatic detector of
343 mother and fetal motion artifact and respiration interference in EHG recording, could be used to develop a
344 preterm labor prediction system in real time based on EHG and therefore may facilitate the translation of the
345 EHG technique to clinical praxis.

346 **Ethical approval:** “All procedures performed in studies involving human participants were in accordance
347 with the ethical standards of the institutional and/or national research committee and with the 1964 Helsinki
348 declaration and its later amendments or comparable ethical standards.”

349 REFERENCES

- 350 1. Aboy M, Cuesta-Frau D, Austin D, Micó-Tormos P (2007) Characterization of sample entropy in the
351 context of biomedical signal analysis. *Annu Int Conf IEEE Eng Med Biol - Proc* 5942–5945. doi:
352 10.1109/IEMBS.2007.4353701
- 353 2. Aboy M, Hornero R, Abásolo D, Álvarez D (2006) Interpretation of the Lempel-Ziv complexity
354 measure in the context of biomedical signal analysis. *IEEE Trans Biomed Eng* 53:2282–2288. doi:
355 10.1109/TBME.2006.883696
- 356 3. Chkeir A, Fleury MJ, Karlsson B, et al (2013) Patterns of electrical activity synchronization in the
357 pregnant rat uterus. *Biomed* 3:140–144. doi: 10.1016/j.biomed.2013.04.007
- 358 4. Crandon AJ (1979) Maternal anxiety and neonatal wellbeing. *J Psychosom Res* 23:113–115. doi:
359 10.1016/0022-3999(79)90015-1
- 360 5. Devedeux D, Marque C, Mansour S, et al (1993) Uterine electromyography: A critical review. *Am J*
361 *Obstet Gynecol* 169:1636–1653. doi: 10.1016/0002-9378(93)90456-S
- 362 6. Fele-Žorž G, Kavšek G, Novak-Antolič Ž, Jager F (2008) A comparison of various linear and non-
363 linear signal processing techniques to separate uterine EMG records of term and pre-term delivery
364 groups. *Med Biol Eng Comput* 46:911–922. doi: 10.1007/s11517-008-0350-y
- 365 7. Fergus P, Cheung P, Hussain A, et al (2013) Prediction of Preterm Deliveries from EHG Signals Using
366 Machine Learning. *PLoS One*. doi: 10.1371/journal.pone.0077154

- 367 8. Garfield RE, Maner WL (2006) Biophysical methods of prediction and prevention of preterm labor:
368 uterine electromyography and cervical light-induced fluorescence – new obstetrical diagnostic
369 techniques. In: Preterm Birth. pp 131–144
- 370 9. Garfield RE, Maner WL (2007) Physiology and electrical activity of uterine contractions. *Semin Cell*
371 *Dev Biol* 18:289–295. doi: 10.1016/j.semcdb.2007.05.004
- 372 10. Garfield RE, Maner WL, MacKay LB, et al (2005) Comparing uterine electromyography activity of
373 antepartum patients versus term labor patients. *Am J Obstet Gynecol* 193:23–29. doi:
374 10.1016/j.ajog.2005.01.050
- 375 11. Goldenberg RL, Culhane JF, Iams JD, Romero R (2008) Epidemiology and causes of preterm birth.
376 *Lancet* 371:75–84. doi: 10.1016/S0140-6736(08)60074-4
- 377 12. Gynecologists AC of O and (2012) ACOG practice bulletin no. 127: Management of preterm labor.
378 *Obstet Gynecol* 119:1308–1317. doi: 10.1097/AOG.0b013e31825af2f0
- 379 13. Hadar E, Biron-Shental T, Gavish O, et al (2015) A comparison between electrical uterine monitor,
380 tocodynamometer and intra uterine pressure catheter for uterine activity in labor. *J Matern Neonatal*
381 *Med* 28:1367–1374. doi: 10.3109/14767058.2014.954539
- 382 14. Hans P, Dewandre P, Brichant JF, Bonhomme V (2005) Comparative effects of ketamine on Bispectral
383 Index and spectral entropy of the electroencephalogram under sevoflurane anaesthesia. *Br J Anesth*
384 94:336–340. doi: 10.1093/bja/aei047
- 385 15. Hassan M, Terrien J, Marque C, Karlsson B (2011) Comparison between approximate entropy,
386 correntropy and time reversibility: Application to uterine electromyogram signals. *Med Eng Phys*
387 33:980–986. doi: 10.1016/j.medengphy.2011.03.010
- 388 16. Hassan M, Terrien J, Muszynski C, et al (2013) Better pregnancy monitoring using nonlinear
389 correlation analysis of external uterine electromyography. *IEEE Trans Biomed Eng* 60:1160–1166.
390 doi: 10.1109/TBME.2012.2229279
- 391 17. Horoba K, Jezewski J, Matonia A, et al (2016) Early predicting a risk of preterm labour by analysis of

- 392 antepartum electrohysterographic signals. *Biocybern Biomed Eng* 36:574–583. doi:
393 10.1016/j.bbe.2016.06.004
- 394 18. Lawn JE, Wilczynska-Ketende K, Cousens SN (2006) Estimating the causes of 4 million neonatal
395 deaths in the year 2000. *Int J Epidemiol* 35:706–718. doi: 10.1093/ije/dyl043
- 396 19. Lemancewicz A, Borowska M, Kuć P, et al (2016) Early diagnosis of threatened premature labor by
397 electrohysterographic recordings - The use of digital signal processing. *Biocybern Biomed Eng*
398 36:302–307. doi: 10.1016/j.bbe.2015.11.005
- 399 20. M L, WL M, LR C (2012) Noninvasive Uterine Electromyography For Prediction of Preterm Delivery.
400 *Am J Obs Gynecol* 204:1–20. doi: 10.1016/j.ajog.2010.09.024.Noninvasive
- 401 21. Maner WL, Garfield RE (2007) Identification of human term and preterm labor using artificial neural
402 networks on uterine electromyography data. *Ann Biomed Eng* 35:465–473. doi: 10.1007/s10439-006-
403 9248-8
- 404 22. Maner WL, Garfield RE, Maul H, et al (2003) Predicting Term and Preterm Delivery With
405 Transabdominal Uterine Electromyography. *Obstet Gynecol* 101:1254–1260. doi: 10.1016/S0029-
406 7844(03)00341-7
- 407 23. Marque C, Gondry J (1999) Use of the electrohysterogram signal for characterization of contractions
408 during pregnancy. *IEEE Trans Biomed Eng* 46:1222–1229.
- 409 24. Maul H, Maner WL, Olson G, et al (2004) Non-invasive transabdominal uterine electromyography
410 correlates with the strength of intrauterine pressure and is predictive of labor and delivery. *J Matern*
411 *Neonatal Med* 15:297–301. doi: 10.1080/14767050410001695301
- 412 25. Most O, Langer O, Kerner R, et al (2008) Can myometrial electrical activity identify patients in
413 preterm labor? *Am J Obstet Gynecol* 199:378. doi: 10.1016/j.ajog.2008.08.003
- 414 26. Petrou S (2005) The economic consequences of preterm birth during the first 10 years of life. *BJOG An*
415 *Int J Obstet Gynaecol* 112:10–15. doi: 10.1111/j.1471-0528.2005.00577.x

- 416 27. Rabotti C, Sammali F, Kuijsters N, et al (2015) Analysis of uterine activity in nonpregnant women by
417 electrohysterography: A feasibility study. In: Proc. Annu. Int. Conf. IEEE Eng. Med. Biol. Soc.
418 EMBS. pp 5916–5919
- 419 28. Schlembach D, Maner WL, Garfield RE, Maul H (2009) Monitoring the progress of pregnancy and
420 labor using electromyography. *Eur J Obstet Gynecol Reprod Biol* 144:2–8. doi:
421 10.1016/j.ejogrb.2009.02.016
- 422 29. Sikora J, Matonia A, Czabański R, et al (2011) Recognition of premature threatening labour symptoms
423 from bioelectrical uterine activity signals. *Arch Perinat Med* 17:97–103.
- 424 30. Vinken MPGC, Rabotti C, Mischi M, et al (2010) Nifedipine-induced changes in the
425 electrohysterogram of preterm contractions: feasibility in clinical practice. *Obstet Gynecol Int*
426 2010:325635. doi: 10.1155/2010/325635
- 427 31. Vrhovec J, Lebar AM (2012) An Uterine Electromyographic Activity as a Measure of Labor
428 Progression. *Appl EMG Clin Sport Med* 243–268. doi: 10.5772/25526
- 429 32. Vrhovec J, Macek-Lebar A, Rudel D (2007) Evaluating Uterine Electrohysterogram with Entropy.
430 11th Mediterr Conf Med Biomed Eng Comput 144–147. doi: 10.1007/978-3-540-73044-6_36
- 431 33. Ye-Lin Y, Bueno-Barrachina JM, Prats-boluda G, et al (2017) Wireless sensor node for non-invasive
432 high precision electrocardiographic signal acquisition based on a multi-ring electrode. *Measurement*
433 97:195–202. doi: 10.1016/j.measurement.2016.11.009
- 434 34. Ye-Lin Y, Garcia-Casado J, Prats-Boluda G, et al (2014) Automatic identification of motion artifacts
435 in EHG recording for robust analysis of uterine contractions. *Comput Math Methods Med*. doi:
436 10.1155/2014/470786
- 437 35. Zhang XS, Roy RJ, Jensen EW (2001) EEG complexity as a measure of depth of anesthesia for
438 patients. *IEEE Trans Biomed Eng* 48:1424–1433. doi: 10.1109/10.966601

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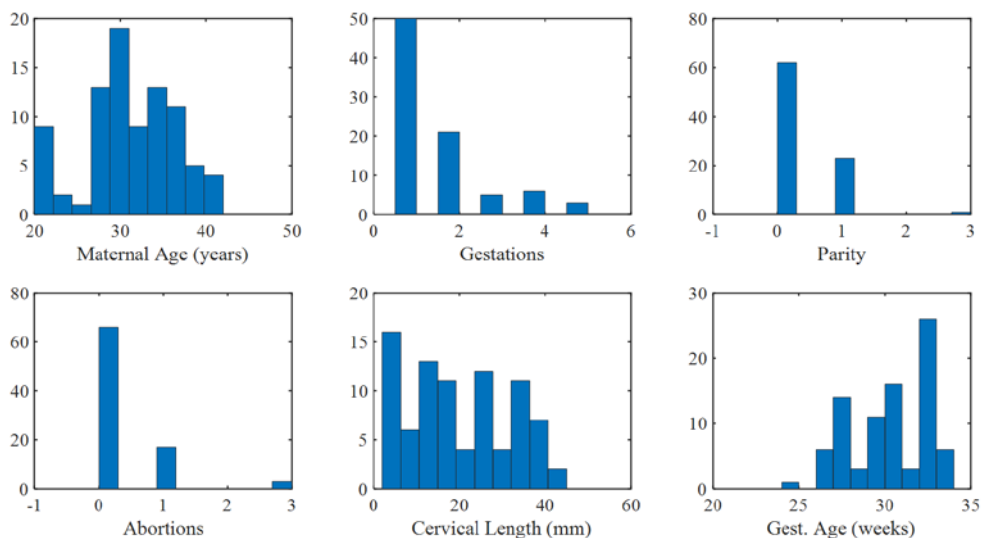
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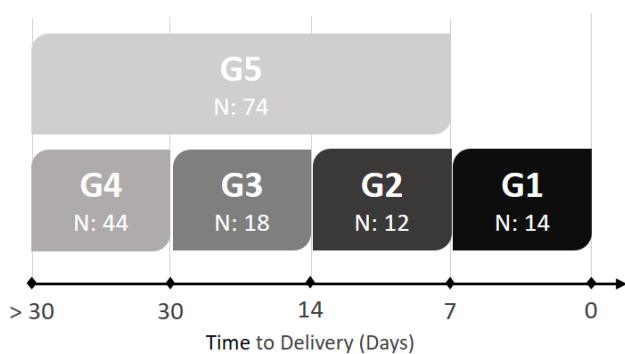
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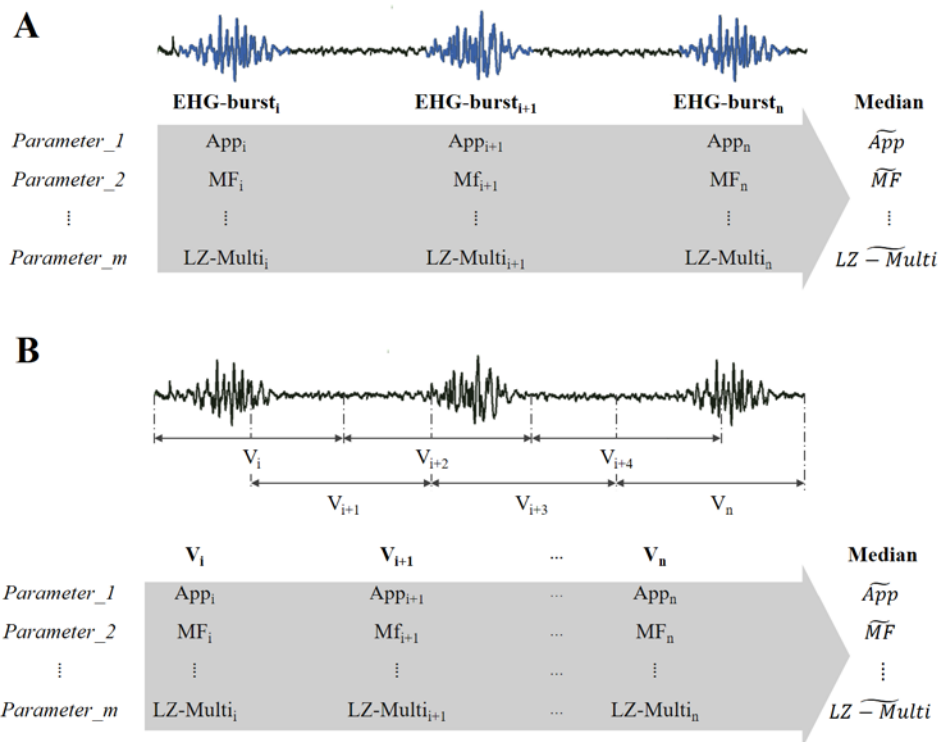
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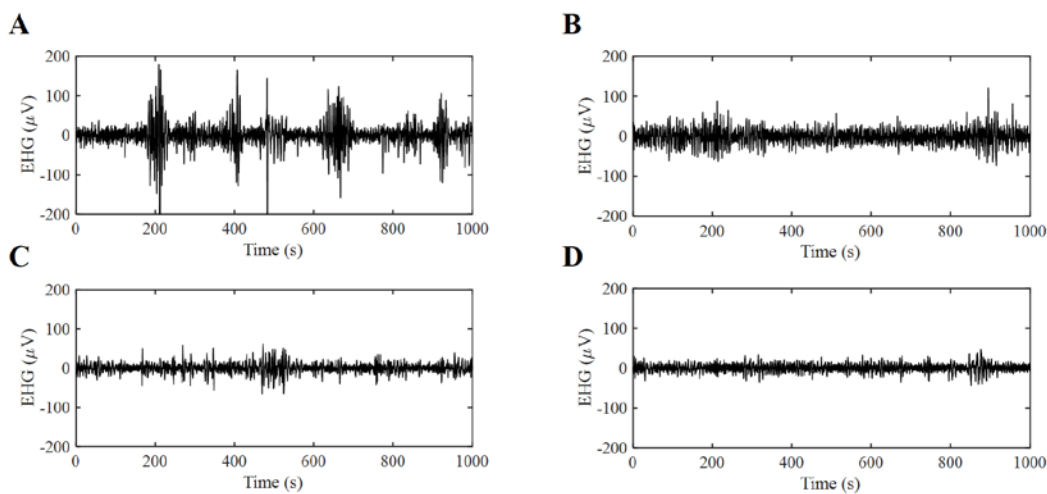
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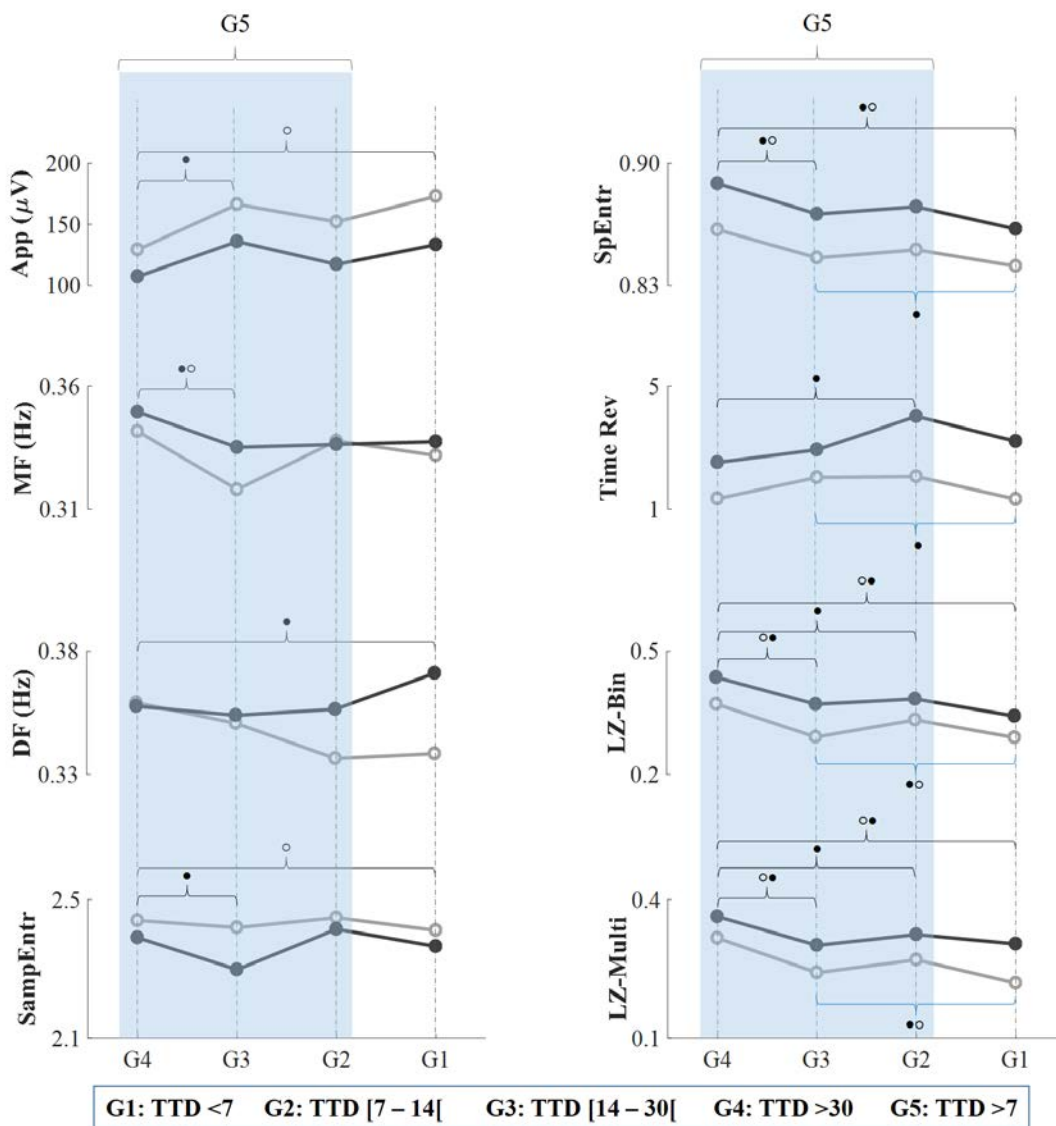
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 482 significant differences between the rest of the groups.



483

484

485 Table 1: Patients' Obstetrical information.

		G1	G2	G3	G4	G5
		<7 days	[7-14[[14-30[>30 days	>7 days
Maternal Age (years)		30.9 ± 4.7	25.7 ± 4.9	33.6 ± 3.9	31.3 ± 5.4	26.7 ± 9.9
Gestations		2.0 ± 1.5	1.5 ± 1.1	1.7 ± 0.9	1.6 ± 0.7	1.62 ± 1.14
Parity		0.4 ± 0.9	0.3 ± 0.4	0.4 ± 0.5	0.3 ± 0.4	0.32 ± 0.62
Abortions		0.33 ± 0.89	0.27 ± 0.47	0.22 ± 0.43	0.28 ± 0.45	0.26 ± 0.41
Cervical Length (mm)		9.8 ± 6.5	13.1 ± 5.8	25.6 ± 10.6	21.9 ± 13.4	19.3 ± 14.6
Gest. Age (weeks)		32.0 ± 2.5	31.1 ± 2.2	32.3 ± 1.4	29.7 ± 2.1	31.8 ± 2.2
ATB (Tocolytic) Classification. Number of records	Without	1	0	0	6	6
	Under	4	5	6	15	26
	Post	9	7	12	23	42
	Total	14	12	18	44	74

486

487 Table 2. Mean and standard deviation of EHG-bursts' parameters in each group.

	<i>G1</i>	<i>G2</i>	<i>G3</i>	<i>G4</i>	<i>G5</i>
<i>App</i> (μ V)	188.2 \pm 95.6	159.3 \pm 63.0	176.1 \pm 57.6	136.1 \pm 63.0	151.1 \pm 63.1
<i>MF</i> (Hz)	0.312 \pm 0.03	0.317 \pm 0.02	0.305 \pm 0.03	0.330 \pm 0.04	0.318 \pm 0.03
<i>DF</i> (Hz)	0.349 \pm 0.03	0.344 \pm 0.04	0.360 \pm 0.03	0.366 \pm 0.04	0.364 \pm 0.04
<i>SampEntr</i>	2.32 \pm 0.71	2.45 \pm 0.03	2.32 \pm 0.30	2.41 \pm 0.15	2.39 \pm 0.20
<i>SpEntr</i>	0.846 \pm 0.027	0.854 \pm 0.011	0.850 \pm 0.030	0.862 \pm 0.022	0.861 \pm 0.02
<i>Time Rev</i>	2.17 \pm 5.8	2.59 \pm 1.05	2.25 \pm 1.41	2.14 \pm 2.56	2.28 \pm 2.08
<i>LZ-Bin</i>	0.29 \pm 0.05	0.32 \pm 0.04	0.30 \pm 0.07	0.38 \pm 0.07	0.35 \pm 0.07
<i>LZ-Multi</i>	0.22 \pm 0.07	0.27 \pm 0.03	0.25 \pm 0.06	0.32 \pm 0.07	0.29 \pm 0.07

488

489 Table 3. Mean and standard deviation of EHG complete record analysis parameters in each group.

	<i>G1</i>	<i>G2</i>	<i>G3</i>	<i>G4</i>	<i>G5</i>
<i>App</i> (μ V)	144.9 \pm 74.5	129.5 \pm 61.5	145.2 \pm 47.1	128.1 \pm 92.6	132.5 \pm 78.9
<i>MF</i> (Hz)	0.322 \pm 0.02	0.316 \pm 0.02	0.331 \pm 0.02	0.348 \pm 0.02	0.332 \pm 0.02
<i>DF</i> (Hz)	0.373 \pm 0.03	0.359 \pm 0.01	0.356 \pm 0.01	0.367 \pm 0.03	0.360 \pm 0.02
<i>SampEntr</i>	2.17 \pm 0.34	2.35 \pm 0.2	2.14 \pm 0.37	2.33 \pm 0.17	2.28 \pm 0.25
<i>SpEntr</i>	0.867 \pm 0.016	0.875 \pm 0.010	0.876 \pm 0.025	0.891 \pm 0.020	0.88 \pm 0.02
<i>Time Rev</i>	3.44 \pm 1.81	4.31 \pm 1.10	3.20 \pm 1.49	2.89 \pm 1.55	3.62 \pm 1.52
<i>LZ-Bin</i>	0.36 \pm 0.05	0.38 \pm 0.03	0.39 \pm 0.07	0.44 \pm 0.07	0.42 \pm 0.07
<i>LZ-Multi</i>	0.30 \pm 0.04	0.32 \pm 0.02	0.31 \pm 0.05	0.35 \pm 0.05	0.34 \pm 0.05

490

491

Brief biography

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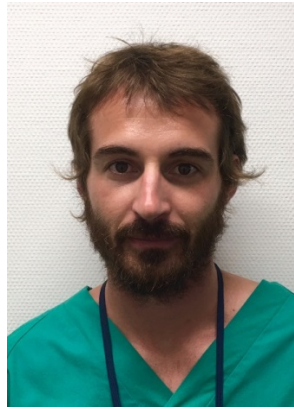
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