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Additional Information

24 Sensitive precise measurements were taken (high signal-to-noise ratios, 10- μ m image
25 resolution, 99% scan-to-scan reproducibility). These features confirmed their potential as
26 analytical tools, are a competitive alternative to fluorescence scanners, and incorporate
27 additional advantages, such as user-friendly interface and connectivity for telemedicine needs.
28 The analytical performances of the integrated platform (assay and reader) in the human samples
29 were also excellent, with a low detection limit (100 genomic DNA copies), and reproducible
30 (<15%) and cheap assays (< 10 €/test). The correct genotyping of a genetic biomarker (single-
31 nucleotide polymorphism located in the **GRIK4** gene) was achieved as the assigned genotypes
32 agreed with those determined by using sequencing. The portability, favourable discriminating
33 and read-out capabilities reveal that the implementation of mass-produced low-cost devices
34 into minimal-specialised clinical laboratories is closer to becoming a reality.

35

36 **Keywords**

37 Single-nucleotide polymorphism; Isothermal DNA amplification; Point-of-care testing;
38 Smartphone; Scanner; Compact disc.

39

40 INTRODUCTION

41 Advanced molecular technologies are a growing field in the healthcare system that
42 address both diagnostics and treatment selection [1]. Current analytical methodologies enable
43 measurements, basically in laboratories with specialised infrastructure and classical
44 instruments (biochemical analysers, DNA sequencers, scanners, etc.). Alternative systems are
45 needed to broaden the clinical facilities available to incorporate diagnostic tools. Point-of-care
46 (POC) approaches offer fast, robust and reliable results and reduce medical costs, mislabelling
47 and mishandling [2]. Thanks to these characteristics, POC tests are used for the prevention,
48 control of disease outbreaks and monitoring health conditions, extending the medical scenarios
49 to be addressed [3].

50 The recent advances made in materials, microfluidics and instrumentation have improved
51 the performances of POC systems [4]. Particularly, the availability and affordability of
52 consumer electronic, or home electronic, equipment, are increasing the possibilities of
53 innovative solutions. They include devices used for entertainment, communications and home-
54 office activities, such as smartphones, scanners, and compact disc drives. These hand-held
55 optoelectronic devices have the potential to make biosensing more accessible to society [5].
56 Two categories can be defined depending on the employed sensing principle. The first is
57 composed of digital imaging devices, which consists of an array of pixel sensors that converts
58 light intensity into electrical current (charge coupled device or a complementary-metal-oxide-
59 semiconductor). The optical sensors installed in smartphones [6], documental scanners [7], or
60 similar devices, provide images of the assay platform, generally a planar or microfluidic chip,
61 with enough quality to obtain analytical information [8]. In case of smartphones, custom-made
62 attachments are used to hold the sample and auxiliary optical modules [9]. The second category
63 is based on compact disc technology, where assays are performed on the optical disc surface
64 and a disc drive acts as the optical scanner [10-13].

65 Consumer electronic equipment has been adapted as imaging platforms for genetic
66 diagnoses with demonstrated sensitivity [14]. To reach the copy number required for molecular
67 detection, a common challenge is the DNA amplification process (e.g. polymerase chain
68 reaction, PCR). In POC approaches, one important component is the heat system for
69 performing a precise fast thermal cycling [15]. In recent years, alternative methods have been
70 explored using isothermal amplification techniques and simple heaters [16, 17]. Among the
71 available options, the loop-mediated amplification method (LAMP) is the most popular
72 solution [18]. This reaction amplifies DNA at constant temperatures by using the Bst
73 polymerase large fragment, which presents great strand displacement activity and enzymatic
74 processivity. LAMP also provides higher amplification yields than PCR in shorter incubation
75 times.

76 Regarding applications, consumer electronic devices have been employed for detecting
77 specific target (e.g. disease biomarker and infectious pathogen) [19-22]. However, several
78 diagnostic and prognostic applications demand the simultaneous detection of multiple regions
79 or variants (e.g. differentiation among similar pathogen strains or detection of point-mutations).
80 In order to increase multiplexing capabilities, a common strategy is multiple parallel assays
81 performed in microreactors on chips [23]. Another alternative is the combination with a
82 hybridisation assay using probes immobilised on a chip surface, followed by adequate labelling
83 and the optical detection of the corresponding array. In a recent paper, we demonstrated the
84 potential of this approach combined to smartphone based-detection [24]. However, other
85 consumer electronic devices are also potentially compatible to be used as readers of array-
86 based assays. A scientific challenge for low-cost diagnostic community is an evaluation of their
87 suitability and limitations, considering specific spectral responsivity, integration capabilities
88 and associated data quality [25].

89 In this research, our goal was to explore the analytical capabilities of different consumer
90 electronic techniques leverages for imaging of array chips of nucleic acids. The compared
91 devices were smartphone, flatbed scanner, USB digital microscope and compact disc drive.
92 Therefore, the study was to establish the feasible requirements to transform each equipment into
93 analytical reader of results generated by a highly sensitive and specific isothermal DNA assay.
94 As proof of concept, the final POC integrated systems (biosensing assay and readers) were
95 intended to be applied to the accurate low-cost discrimination of clinically relevant genetic
96 variants.

97

98 MATERIAL AND METHODS

99 Primers and probes

100 The studied biomarker was the single nucleotide polymorphism (SNP) associated with
101 the pharmacogenomics of anti-depressants drugs (rs1954787, g.285909T>C, located in the
102 GRIK4 gene). LAMP primers and probes were selected according to the thermodynamic
103 parameters associated with the perfect-match and mismatched duplexes ([Supplementary](#)
104 [Material](#)). All the oligonucleotides used in this study were purchased from Eurofins
105 (Luxembourg).

106

107 LAMP combined with allele selective hybridization

108 Genomic DNA amplification was carried out in 200- μ L polypropylene vials. Each
109 reaction (12.5 μ L) was composed of 1 μ L isothermal amplification buffer (20 mM Tris-HCl, 10
110 mM $(\text{NH}_4)_2\text{SO}_4$, 50 mM KCl, 2 mM MgSO_4 , 0.1% Tween 20, pH 8.8), 1.5 M betaine,
111 additional 6 mM MgSO_4 , 1.2 mM dNTPs, 10 μ M digoxigenin-11-deoxyuridine triphosphate
112 (DIG-dUTP), 0.2 μ M of outer primers, 1.2 μ M of inner primers, 0.32 U/ μ L Bst polymerase 2.0

113 (New England Biolabs, USA) and 0.32 ng/μL of DNA. Vials were incubated at 62 °C for 60
114 min (digital heat block, VWR, USA).

115 An allele-selective hybridisation assay led to the discrimination of the amplified
116 products. Assays were performed on polycarbonate planar slides (detection device: chip-based
117 sensors) or on the bottom layer of DVD discs (detection device: DVD drive). Probe arraying
118 and the hybridisation of the amplification products were performed according to the protocol
119 developed in previous work [26]. The array layout contained 4 replicates per probe and 10
120 arrays per chip. Regarding chip staining, the digoxigenin-labelled duplexes were recognised
121 by horseradish-peroxidase-conjugated anti-digoxigenin antibodies, and were stained by
122 deposition of 3,3',5,5'-tetramethylbenzidine (ep(HS)TMB, SDT reagents, Germany).

123

124 Array imaging

125 Four different consumer electronic technologies were examined to image the arrays
126 according to the following protocols:

127 USB digital microscope The profile intensities were measured by a portable microscope
128 (Dino-Lite AM4013MZT, AnMo Electronics Co., Taiwan) based on a colour CMOS system
129 (resolution 1.3 Megapixel, maximum frame rate: 30 fps). Images were captured by vertically
130 positioning the equipment over the array at a 5-centimetre distance and employing the
131 microscope internal LED as the light source (maximum illumination 18,500 lux). The
132 DinoCapture 2.0 software was employed to record the image at the 1.3-megapixel resolution.

133 Smartphone Array images were also captured by a smartphone (MotoG first generation,
134 Motorola, EEUU) using a home-made chamber (8 x 6.7 x 4.4 cm) [24]. The device
135 specifications were typical of a mid-range phone (display 4.5", processor 1.2 GHz quad core,
136 RAM 1 GB, rear camera 5-megapixel CMOS). The reading chamber had a frontal rectangular
137 aperture for the smartphone camera, a lateral hole used to illuminate the array by an external

138 optical fibre light source (power 20W, LE.5209 model, Euromex, Holland), and an aperture for
139 inserting the assay chip. After adjusting the focus and exposure (75% level), images were
140 captured. The system did not require any connection to the telephone network.

141 Flatbed scanner An office scanner (Perfection 1640SU Office, Epson, Japan), which
142 incorporated a CCD image sensor, was also employed in the reflectance mode. The array
143 support was positioned over the equipment bed and scanning was carried out at a 1,600 dpi
144 (dots per inch) resolution using the Epson scan default software (disabled auto-correction
145 functions).

146 Compact disc drive. The DVD-supported microarrays were directly read by a digital
147 versatile disc (DVD) drive (LG DVD GSA-H42N, LG Electronics Inc., USA), which
148 incorporated a data acquisition board model (DT9832A-02-OEM; Data Translation, Marlboro,
149 MA, USA) [13]. The standard disc drive acted as a miniature high-precision optical device that
150 consists of laser diodes, collimating lenses, diffraction gratings and a photodiode. The focus
151 and tracking mechanism was responsible for spinning the disc and moving the optical pickup
152 head unit. The reading conditions were adjusted by a custom software: rotation speed of 4×
153 (13.46 m/s) and 21 dB gain at a detection rate of 1,700 mega-samples/s. Thus, the array image
154 was formed from the data captured in each radius.

155 The ImageJ free-access software (National Institutes of Health, USA) was used to
156 process the images in the tagged image file format (TIF) and on a 16-bit grey-scale (65,535
157 intensity values). The software provided the spot and surrounding background intensities.
158 Signal-to-noise ratios were calculated as the net spot signal, divided by the background
159 standard deviation.

160

161

162 **Sample analysis**

163 The performances of the POC systems for clinical routine were evaluated by applying
164 SNP genotyping methods. Human subjects (n=15) were recruited for the present study
165 according to ethics guidelines. Buccal smear samples were collected by a minimally invasive
166 method. DNA extracts were obtained using a Purelink Genomic DNA mini kit (Thermo Fisher
167 Scientific, USA). The genomic DNA content was quantified with a NanoDrop 2000
168 spectrophotometer (Thermo Fisher Scientific, USA). Extracts were diluted to 4 ng/ μ L (1,300
169 copies) and analysed as described in previous sections. The analysis was declared valid if the
170 amplification and hybridisation controls provided a correct response. The genotype decision
171 rule was constructed based on the signal-to-noise ratio associated with the wild-type (T) and
172 mutant (C) probes.

173

174 **Genotyping validation**

175 Sanger sequencing was used to determine patient genotypes (blind samples). Each PCR
176 reaction (12.5 μ L) contained 1x amplification buffer, 3 mM MgCl₂, 200 μ M dNTPs, 300 nM
177 of forward and reverse primers, 0.5 units of Taq polymerase (Biotools, Spain) and 4 ng of
DNA. The amplification was carried out in a thermal cycler (

1 **Consumer electronics devices for DNA**
2 **genotyping based on loop-mediated isothermal**
3 **amplification and array hybridization**

4
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13
14 **ABSTRACT**

15 Consumer electronic technologies offer practical performances to develop compact
16 biosensing systems intended for the point-of-care testing of DNA biomarkers. Herein a
17 discrimination method for detecting single nucleotide polymorphisms, based on isothermal
18 amplification and on-chip hybridisation, was developed and integrated into user-friendly
19 optical devices: e.g., USB digital microscope, flatbed scanner, smartphone and DVD drive. In
20 order to adequately identify a single base change, loop-mediated isothermal amplification
21 (LAMP) was employed, with high yields (8 orders) within 45 min. Subsequently, products
22 were directly hybridised to the allele-specific probes attached to plastic chips in an array
23 format. After colorimetric staining, four consumer electronic techniques were compared.