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Additional Information

Evaluation of the engineering performance of different bio-based aliphatic homopolyamide tubes prepared by profile extrusion

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ABSTRACT. In the present study, three different commercial bio-based polyamides (bio-PAs), namely polyamide 610 (PA610), polyamide 1010 (PA1010), and polyamide 1012 (PA1012), were processed by profile extrusion with an annular die. These aliphatic homopolyamides, also known as “green nylons”, are industrially produced by polycondensation reaction of diamines and dicarboxylic acids that are partially or fully obtained from naturally occurring castor oil. The profile-extruded bio-PA tubes were characterized and compared in terms of their thermal, thermomechanical, and mechanical properties and water uptake. Resultant comparative evaluation indicated that both the methylene-to-amide (CH₂/CONH) ratio and the crystallinity degree of the bio-PAs played the main role in determining the tube properties. Due to significant differences in their CH₂/CONH ratio, the PA610 tubes showed the highest thermal performance while the tubes made of PA1012 tubes presented the highest flexibility and lowest water uptake. Interestingly, the fully bio-based PA1010 tubes offered the most balanced and enhanced engineering performance, which was ascribed to the high crystallinity achieved during profile extrusion. The here-developed bio-PA tubes can fulfil demanding technical requirements and these also certainly represent a sustainable answer to the rising demand for new high-performance biopolymers for engineering applications

KEYWORDS Green nylons; Methylene-to-amide ratio; Plastics engineering; Structure-property relationships; Tubing extrusion

30 **1. Introduction**

31 Polyamides are polymers, generally linear and semi-crystalline, with recurring amide groups as
32 an integral part of the main polymer chain. These are commonly known in the plastics industry
33 as “nylons”, which are referred to any polyamide having less than 85% of the amide groups
34 directly connected to two aromatic groups [1]. Discovered by Wallace Carothers and early
35 commercialized in the 1940s by DuPont, polyamides can be either obtained by ring-opening
36 polymerization (ROP) of lactams, *i.e.* their bi-functional monomer, or polycondensation, *i.e.*
37 condensation polymerization of diamines and diacids at elevated temperature [2]. The latter
38 reaction is based on a “nylon salt” solution, where the corresponding salt is previously formed
39 at room temperature using a molar ratio dicarboxylic acid/diamine 1:1. The amide group, along
40 with its essential structural role, contributes to the extraordinary mechanical strength and
41 thermal resistance of polyamides due to its polar nature and high chemical stability. As a result,
42 these thermoplastic materials are traditionally considered as “engineering plastics”, being
43 currently manufactured for a wide variety of technically demanding applications such as fibers
44 for clothing for carpets, injection-molded car parts, oil delivery lines and gas pressure pipes,
45 barrier films for food packaging, and soles for high-quality sports shoes [3]. Nowadays, the
46 global plastics market annually requires over 6 million tons of polyamides with a growing rate
47 close to 5% [4]. Traditional polyamide 6 (PA6) and polyamide 66 (PA66), and recently
48 polyamide 12 (PA12), constitute more than 90% of their overall usage in the plastics industry
49 [5].

50 Even though high-performance plastics are classical petrochemistry products, polymer chains
51 can also be partially or completely synthesized from bio-based components [6]. In particular,
52 the development of a sustainable route to the production of bio-based polyamides (bio-PAs) has
53 recently received a high interest due to the growing awareness of the damage sustained by
54 environment [7]. In particular, the synthesis of both traditional and new polyamides from
55 renewable resources could exceptionally reduce high amounts of fossil energy, which is
56 particularly favorable in the light of the growing shortage and rising price of fossil resources[8].
57 Unfortunately, the use of fully bio-PAs, excluding polypeptides and proteins, is still restricted

58 due to the limited availability of renewable diamines [9]. Thus, increasing the applications of
59 bio-PAs is certainly of major interest.

60 Without doubt, castor oil is nowadays playing the biggest role as the raw material to yield the
61 building blocks for the production of bio-PAs [10]. This is a natural, viscous, pale yellow, non-
62 volatile, and non-drying oil with an unusual homogeneous composition. Structurally, castor oil
63 contains 85–95% ricinoleic acid, a 18-carbon (C18) fatty acid, which is available in its
64 triglyceride ester [11]. The oil is obtained from the seed of the *Ricinus communis* plant, which
65 belongs to the family Euphorbiaceae and predominantly grows in the wild of tropical and
66 subtropical countries (*e.g.* Africa, India, Brazil, and China) [12]. Castor oil is not only a
67 naturally occurring resource, but it is also inexpensive and environmentally friendly. Due to its
68 extreme drought resistance, the plant is primarily cultivated in sites that are unsuitable for food
69 production so that it does not compete directly with food purposes [13]. It is estimated that over
70 600,000 metric tons of castor oil are annually produced, of which at least one third are currently
71 used for the synthesis of bio-PAs [14].

72 Ricinoleic acid is the starting compound for the different bio-routes, which is obtained by
73 subjecting castor oil either to a transesterification step or a saponification step [15]. Sebacic acid,
74 *i.e.* 1,10-decanedioic acid, is manufactured by heating ricinoleic acid to high temperatures,
75 typically about 250°C, with alkali [16]. Although its manufacturing yields are lower than those
76 of current petrochemical monomers used in the synthesis of traditional polyamides, this route
77 has been found to be cost competitive [17]. The C10 dicarboxylic acid can readily react with
78 petroleum-based 1,6-hexamethylene diamine (HMDA), obtained from butadiene, *via*
79 polycondensation to produce aliphatic polyamide 610 (PA610). As a result, PA610 is typically
80 60–63 wt.-% based on natural resources [18]. Sebacic acid can also polymerize with 1,10-
81 decamethylene diamine (DMDA) to produce aliphatic polyamide 1010 (PA1010). Interestingly,
82 DMDA, the C10 diamine, can be obtained by exposing sebacic acid to ammonia followed by
83 dehydration and hydrogenation [19]. Since both monomers are obtained from castor oil,
84 resultant PA1010 is fully bio-based. Finally, aliphatic polyamide 1012 (PA1012) is a
85 polycondensation product of DMDA and 1,12-dodecanedioic acid. The C12 dicarboxylic acid is

86 typically fossil-based, being the bio-based content of PA1012 approximately 45 wt.-%.
87 However, more recently, this has been also obtained from palm kernel oil *via* a biotechnological
88 process [20]. As a result, PA1012 can also consists up to 100 wt.-% of renewable raw materials.
89 **Figure 1** shows the chemical structure of PA610, PA1010, and PA1012, indicating the weight
90 percentage of renewably sourced ingredients. As it can be observed, these bio-PAs consist of
91 amide groups separated by alkane segments of different length, which results in different amide
92 concentration per polymer chain. Therefore, the methylene-to-amide (CH_2/CONH) ratio results
93 in 7, 9 and 10 for PA610, PA1010 and PA1012, respectively. Polyamides with longer aliphatic
94 segments, *i.e.* with higher CH_2/CONH ratios, have reasonably lower amide densities per unit
95 length of chain. Interestingly, the CH_2/CONH ratio, in combination with the chain symmetry, is
96 known to determine the final properties of polyamides [21]. Even-even polyamides form chain-
97 folded sheets in which the amide groups participate in linear hydrogen bonding to one another.
98 Lower CH_2/CONH ratios result in a density increase of hydrogen bonds, which restricts the
99 segmental inter-chain mobility of the long-chain aliphatic methylene groups in the polymer
100 backbone and then increases thermal resistance [21], mechanical strength and abrasive wear
101 performance [22] and, hence, tribological behavior [23]. In addition, hydrogen bonding pulls
102 many of the polyamide chains into more ordered crystalline regions, which further increases the
103 polyamide melting point. In particular, it is considered that resultant hydrogen bonds are able to
104 retain the polyamide chains in an ordered solid phase after the alkane segments have effectively
105 melted [21]. Hydrogen bonding also takes place between polyamide and water or polar
106 absorbed substances, which acts as a plasticizer, lowering the glass transition temperature (T_g)
107 and impairing the mechanical performance significantly [24].

108 Profile extrusion is the high-volume process of making continuous shapes of plastic, ranging
109 from solid to hollow forms, but not including sheet and film. When the polymer melt is
110 extruded through an annular die, round cross-sections such as tubes and pipes are obtained. This
111 is specifically called pipe extrusion or tubing extrusion [25]. During this process, polymer
112 resins, habitually in the form of pellets, flow from the main hopper to the gap between the
113 rotating screw and heated barrel of the extruder. Once the polymer is melted, mixed and

114 pressurized in the extruder, it is then pumped through the annular die. The extruded product,
115 while being pulled, passes through a vacuum sizer in which it attains its final dimensions. This
116 is followed by cooling *via* chilled water immersion or spraying and cutting to fixed lengths.
117 Pipes, with a diameter of 2 m or greater, and tubes, from 10 mm down to below 1 mm, can be
118 processed by profile extrusion [26]. The annular dies used in this process are normally of spider
119 or spiral mandrel design [27].

120 The present study reports, for the first time, the preparation by profile extrusion and
121 characterization of tubes made of three bio-PAs, namely PA610, PA1010, and PA1012. Since
122 the amide group concentration controls the physical properties of aliphatic polyamides, the
123 thermal, thermomechanical, and mechanical performance and water uptake of these bio-PA
124 tubes were evaluated and compared. The obtained results were ascribed to the chemical
125 structure of the bio-PAs, based on different CH₂/CONH ratios, and the processing conditions in
126 which the tubes were obtained.

127 **2. Experimental**

128 **2.1. Materials**

129 PA610 was supplied by DuPont (Solingen, Germany) as medium-viscosity grade Zytel® RS
130 LC4601. This homopolyamide is developed for extrusion applications, has a density of 1.04
131 g/cm³, and contains approximately 60 wt.-% of renewably sourced ingredients. Commercial
132 PA1010 was Grilamid® XE 4181 provided by EMS-Chemie A.G. (Domat/Ems, Switzerland).
133 This is a fully bio-based high-viscosity extrusion-grade homopolyamide with a density of 1.05
134 g/cm³. Finally, PA1012 was Vestamid® Terra DD 2230 (CW1120), distributed by Evonik
135 Industries (Essen, Germany). This is a high-viscosity homopolyamide with a density of 1.03
136 g/cm³ and 45 wt.-% based on bio-renewables. The renewable weight contents were provided by
137 the manufacturers according to ASTM D6866 standard.

138 **2.2. Profile extrusion**

139 Extrusion of tubes was performed using a Collin E30M single-screw extruder equipped with a
140 15-mm annular die based on a spider ring design. The barrel extruder presented a

141 length/diameter (L/D) of 30 and screw speed was 40 rpm. Temperature profile was set
142 accordingly to provide a melt temperature during extrusion of 250°C, for PA610, and 225°C,
143 for PA1010 and PA1012. In all cases die temperature was set at 275°C. The process is
144 illustrated in **Figure 2** showing its different sections. Briefly, the extruded tube exiting the die
145 travelled a short distance in air, allowing a thin skin to form. Then it passed through a vacuum
146 sizing chamber, which was equipped with sizing rings and operated at 230 mbar. The tubes,
147 while being pulled, entered a cooling bath with chilled water at 15°C to dissipate the heat. The
148 pull-out system was a caterpillar-type puller (capstan). Finally, annealing was performed in a
149 reheat station working with an open flame. Line speed was 5 m/min. Tube specimens of
150 different lengths with an outer diameter (OD) of 10 mm and wall thickness of 1 mm were
151 ejected from the cutting station.

152 **2.3. Infrared spectroscopy**

153 Chemical analysis was performed *via* attenuated total reflection–Fourier transform infrared
154 (ATR-FTIR) spectroscopy. Spectra were recorded using a Bruker S.A. Vector 22 (Madrid,
155 Spain) coupled to a PIKE MIRacle™ single reflection diamond ATR accessory (Madison,
156 USA). Data were collected as the average of ten scans from 4000 to 400 cm⁻¹ at a spectral
157 resolution of 4 cm⁻¹.

158 **2.4. Thermal characterization**

159 Thermal transitions were obtained by differential scanning calorimetry (DSC) using a Mettler-
160 Toledo, Inc. (Schwerzenbach, Switzerland) 821 model. For this, *ca.* 5 mg of tube samples were
161 placed in 40- μ l hermetic aluminum sealed pans, previously calibrated with an indium standard.
162 The analysis was performed in a dry reducing atmosphere in which nitrogen flowed at a
163 constant rate of 66 mL/min. Samples were subjected to a two-step regime at a heating rate of 10
164 °C/min to evaluate the thermal transitions. An initial heating scan from 30 to 250°C was
165 followed by a cooling scan to 30°C. The cold crystallization temperature (T_{cc}), normalized cold
166 crystallization enthalpy (ΔH_{cc}), melting temperature (T_m), and normalized enthalpy of melting
167 (ΔH_m) were obtained from the heating scan while the crystallization temperature from the melt

168 (T_c) and normalized enthalpy of crystallization (ΔH_c) were determined from the cooling scan.

169 The percentage of crystallinity (X_c) was determined using the following equation:

$$170 \quad X_c = \left[\frac{\Delta H_m - \Delta H_{cc}}{\Delta H_m^0} \right] \cdot 100 \quad (1)$$

171 Where ΔH_m^0 (J/g) represents the theoretical melt enthalpy of a fully crystalline bio-PA,
172 considering 197 J/g for PA610 [28], 244 J/g for PA1010 [29] and 209.2 J/g for PA1012 [30].

173 Thermal stability was determined by thermogravimetric analysis (TGA) in a TGA/SDTA 851
174 thermobalance from Mettler-Toledo, LLC (Columbus, OH, USA). The heating program was set
175 from 30 to 700°C at a heating rate of 20 °C /min in air atmosphere with a constant flow-rate of
176 66 mL/min. Approximately 5-7 mg of tube sample was used for the measurements. The onset
177 degradation temperature was defined as the temperature at 5% weight loss ($T_{5\%}$) and the
178 degradation temperature (T_{deg}) was obtained from the maximum value of the first derivative.

179 **2.5. Thermomechanical characterization**

180 **Dynamic mechanical thermal analysis (DMTA) was conducted in tension mode using a DMA-1**
181 **from Mettler-Toledo GmbH (Greifensee, Switzerland). Tube samples of 5 mm were cut**
182 **longitudinally into stripes (10x5x1 mm³) and subjected to a temperature program ranging from**
183 **0 to 140°C at a heating rate of 2 °C/min, a deformation frequency of 1 Hz, and a strain of 0.1%.**

184 Vicat softening temperature and heat deflection temperature (HDT) were measured in a
185 Vicat/HDT station VHDT 20 from Metrotec S.A. (San Sebastián, Spain). Vicat values were
186 obtained according ISO 306, following B50 method. This was performed on circular
187 compression-molded samples with a diameter of 2.5 cm and a thickness of 4 mm prepared in a
188 10-Tn hydraulic press from Robima S.A. (Valencia, Spain) equipped with two hot aluminum
189 plates and a temperature controller from Dupra S.A. (Castalla, Spain) [31]. Specimens were cut
190 using a die on a hydraulic press model MEGA KCK-15A from Melchor Gabilondo S.A.
191 (Vizcaya, Spain) [32]. **During this test, each specimen was placed in the testing apparatus so**
192 **that the penetrating needle rested on its surface at least 1 mm from the edge.** The applied force
193 was 50 N and the heating rate was 50 °C/h.

194 Regarding HDT characterization, this was carried out using 80-mm long tubes based on ISO 75.

195 The bio-PA tubes were placed at a distance between supporting edges of 60 mm and a weight of
196 320 g was applied, which corresponds to a pressure of 1.8 MPa. The heating rate was 120 °C/h
197 as recommended in the corresponding standard.

198 Dimensional stability was studied by measuring the coefficient of linear expansion (CLTE)
199 using a thermomechanical analyzer (TMA) Q400 model from TA Instruments (Delaware,
200 USA). Test was performed on 7-mm long tubes. The heating program was set from 0 to 140°C
201 with a constant heating rate of 2 °C/min and a load of 0.02 N. All measurements were done in
202 triplicate.

203 **2.6. Mechanical characterization**

204 Tube specimens with a total length of 150 mm were tested in a universal test machine ELIB 30
205 from S.A.E. Ibertest (Madrid, Spain). Tensile tests were performed according to ISO 527. A 5-
206 kN load cell and a cross-head speed of 5 mm/min were employed. Shore D hardness was
207 determined in a durometer 676-D model from J. Bot S.A. (Barcelona, Spain) following ISO
208 868. All specimens were tested in a controlled chamber at room conditions, *i.e.* 23°C and 50%
209 RH. At least six samples for each material were analyzed and averaged.

210 **2.7. Water uptake measurements**

211 Tube specimens of 80 mm were immersed in distilled water at $23 \pm 1^\circ\text{C}$. Samples were
212 extracted weekly and weighed in an analytical balance with an accuracy of ± 0.1 mg after
213 removing the residual water with a dry cloth. The evolution of water uptake was followed over a
214 whole period of 9 weeks. Measurements were done in triplicate.

215 **3. Results and discussion**

216 **3.1. Visual aspect**

217 **Figure 3** shows the resultant profile-extruded tubes of the here-studied bio-PAs. One can
218 observe in this image that continuous tubes with an OD of 10mm and a homogenous surface
219 were produced. In general, the obtained bio-PA tubes presented high translucency but low

220 transparency, as expected for semi-crystalline polymers. No visual differences among the tubes
221 were noticeable.

222 3.2. Chemical properties

223 **Figure 4** shows the FTIR characteristic absorption peaks of the here-studied bio-based PAs.
224 The broad absorption peak at $\sim 3300\text{ cm}^{-1}$ has been mainly reported for the valence stretch
225 vibrations of hydrogen atoms bonded as N–H of terminal amine groups [33-35]. The intense
226 peaks observed at 2919 and 2851 cm^{-1} are caused from the asymmetric and symmetric C–H
227 stretching vibration of methylene groups, respectively [28]. These peaks were very similar for
228 the three bio-PAs. However, some interesting changes can be observed in these spectra at lower
229 wavenumbers.

230 For the PA1012 and PA1010 the main absorption peak was seen at 1635 cm^{-1} , which has been
231 well assigned to the C=O of Amide I in both α - and β -crystalline phases [29, 34, 35]. This
232 moved down to 1632 cm^{-1} in the case of PA610, which can be either related to its higher amide
233 density or changes in crystallinity. In addition, the strong peak at 1540 cm^{-1} in the spectra of
234 both PA1012 and PA610, which belongs to the bending vibration of N–H in Amide II [34-36],
235 shifted to 1535 cm^{-1} for PA1010. This band displacement to a lower frequency region has
236 recently been ascribed to crystallization increases in polyamides [37]. The band at 1462 cm^{-1}
237 has been related to the contribution of the C–N stretching vibration of amide groups [29] and C–
238 H bending vibration in methylene groups [35]. The group of bands in the range $1300\text{-}1200\text{ cm}^{-1}$
239 are attributed to the gauche nitrogen-methylene group, *i.e.* N–H and C–H twisting [28, 38].
240 These absorption bands, showing a main peak centered at 1238 cm^{-1} , became sharper and more
241 intense in the spectrum of PA1010. This suggests that chain conformation of the methylene
242 sequences in PA1010 was more ordered. The aforementioned changes can be therefore ascribed
243 to the more symmetrical chain structure of PA1010, which favors molecular folding and
244 subsequent crystallization. The low-intense bands at 1160 and 940 cm^{-1} that can be observed for
245 both PA1010 and PA1012 are attributed to the skeletal motion and in-plane modes of CO–NH
246 bonds, respectively, which are characteristic of amide groups in semi-crystalline polyamides

247 [39]. For PA610, this peak shifted towards 922 cm⁻¹. In this sense, the bands located at 936 and
248 922 cm⁻¹ have been attributed to the amide C–C=O vibration stretching that are related to the
249 crystalline and amorphous phases in PA66, respectively [28]. This indicates that the structure of
250 PA610 was predominantly amorphous. Finally, the peak at 720 cm⁻¹ corresponds to the shear
251 vibration of methylene groups, *i.e.* C–H rocking [35]. This was more intense in the spectra of
252 PA1012 and PA1010 than in the PA610 spectrum possibly due to its lower CH₂/CONH ratio.

253 3.3. Thermal properties

254 **Figure 5** includes the heating and cooling DSC scans of the bio-PA tubes and the results
255 obtained from these curves are summarized in **Table 1**. The melting thermograms, gathered in
256 **Figure 5a**, show that all bio-PAs showed T_g values in the range of 40-60°C. However, these
257 were difficult to elucidate, particularly for PA1010 and PA1012, probably due to their reduced
258 amorphous phase. It can also be observed that the bio-PA tubes did not show any cold
259 crystallization peak before melting, which can be related to the efficient cooling conditions and
260 annealing treatment performed in the last stage of profile extrusion.

261 All three bio-PAs presented one intense melting peak, suggesting the presence of a predominant
262 single crystalline form in the tubes that can be ascribed to the slow cooling rate applied during
263 profile extrusion. This observation differentiates the here-evaluated bio-PAs from short-chain
264 polyamides (*e.g.* PA6) that typically exhibit a polymorphism behavior, showing multiple
265 melting peaks of different intensities due to the presence of different crystalline forms where
266 distinct crystalline lamellae coexist, *i.e.* α, β, and γ [40]. In particular, the α-form is the most
267 stable and perfect crystalline phase, in which hydrogen bonds are formed between antiparallel
268 chains, stretching to a lower extent the rotation of the polymer chains and, therefore, increasing
269 chains packing [41]. However, one can also observe that the melting peaks were relatively
270 broad, showing the presence of a shoulder at lower temperatures. This was particularly
271 noticeable for PA610, which can denote the presence of an additional crystallite population.
272 According to Thompson-Gibbs relationship, this reflects the melt recrystallization of less

273 perfect crystals, which has been well reported for either conventional polyamides (e.g. PA6,
274 PA66) [42, 43] but also for newly PA610 [36] and PA1010 [44].

275 Due to its lower CH₂/CONH ratio, PA610 presented the highest value of T_m (~215°C) while
276 PA1010 and PA1012 melted at approximately 195 and 183°C, respectively. Therefore, the here-
277 studied bio-PAs followed perfectly correlation between melting temperature and CH₂/CONH
278 ratio. For instance, a similar melting point for PA1012 has been recently reported [45].
279 Regarding PA1010, this melting point has been precisely ascribed to the above-described α-
280 form crystals, which are based on a triclinic system [44]. This value certainly places the thermal
281 properties of these bio-PAs in between those of conventional medium- or long-chain PA12
282 (~179°C) [46] and short-chain PA6 (~221°C) [47]. Furthermore, as commented above, the
283 melting peaks of PA1010 and PA1012 were clearly sharper than that of PA610.

284 **Figure 5b** shows the DSC thermograms taken during the cooling scan. All bio-PAs crystallized
285 from the melt in a single peak according to their CH₂/CONH ratio too. In particular, values of T_c
286 were observed at 182, 177, and 163°C for PA610, PA1010, and PA1012, respectively. It can be
287 observed that PA1010 presented the highest X_c value (~27%) while PA610 showed the lowest
288 (~8%), even though the latter is based on a shorter chain structure, *i.e.* its amide density per
289 chain is higher [24]. The larger crystallinity degree observed for PA1010 can be related to its
290 more symmetrical chain structure in which the diamine and dicarboxylic acid are both based on
291 a C10 chemical structure. This can potentially result in a high regular spacing of the amide
292 groups along the polymer chains that, in turns, favors the formation of orderly regions of
293 crystallinity. In relation to the crystallinity degree observed for PA1012 (~16%), which was
294 higher than PA610 but lower than PA1010, this can be explained by a decrease in the average
295 number of inter-chain hydrogen bonds caused by the increase of the diacid chain length [28].

296 **Table 1** also includes thermal stability values of the profile-extruded bio-PA tubes. All samples
297 presented similar values of thermal degradation. No moisture content was observed in the
298 samples since any noticeable weight loss was observed below 100°C. In particular, the bio-PA
299 tubes remained stable up to approximately 320-340°C, showing a T_{deg} of *ca.* 460°C. Similar
300 thermal degradation profiles in bio-PAs have been previously reported [44, 48]. It was

301 particularly indicated that this mainly involves a β -C-H transfer reaction mechanism,
302 producing ketoamides as the primary decomposition products [49].

303 3.4. Thermomechanical properties

304 **Figure 6** presents the temperature dependence of the storage modulus (G') and damping factor
305 ($\tan \delta$) of the bio-PA tubes. It can be clearly observed in **Figure 6a** that, as temperature
306 increased, the storage modulus gradually decreased. At the glassy plateau region, for instance
307 25°C, PA610 displayed higher storage modulus (~1225 MPa) than PA1010 (~1030 MPa) and,
308 more significantly, than PA 1012 (~618 MPa). This value was expected due to the lower
309 CH_2/CONH ratio of PA610. However, comparison of the biopolymer tubes in the rubbery
310 plateau region, for instance 100°C, indicated that the storage modulus of PA1010 was
311 considerably higher (~259 MPa) than that observed for both PA1012 (~164 MPa) and PA610
312 (~107 MPa). This interesting observation confirms previous chemical and thermal analyses,
313 indicating that PA610 is a highly amorphous material. As a result, in the rubber-like state, *i.e.*
314 above T_g , mechanical strength of PA610 was considerably reduced. On the contrary, the higher
315 crystallinity of PA1012 and, particularly, of PA1010, potentially restricted the movement of the
316 polymer chains and improved elasticity as temperature is increased.

317 **Figure 6b** shows the damping factor as a function of temperature for the PA610, PA1010, and
318 PA1012 tubes measured by DMTA. A loss peak can be seen in the curves that points out the α -
319 relaxation of the bio-PAs, which is related to their T_g . Due to PA610 presents the lowest
320 CH_2/CONH ratio, *i.e.* the highest amide density, this bio-PA exhibited the highest α -relaxation
321 value (~51 °C). This was followed by PA1010 (~38°C) and PA1012 (~27°C). Therefore, the α -
322 relaxation values perfectly correlated with the CH_2/CONH ratio. In addition, the peak intensities
323 for both PA1010 and PA1012 did not only shift towards lower temperatures but, more
324 importantly, these were also significantly lower than that for PA610. This observation clearly
325 confirms that a lower amount of amorphous part underwent glass transition in both PA1010 and
326 PA1012 when compared to PA610.

327 **Table 2** includes the coefficients of linear thermal expansion (CLTE) of the bio-PA tubes below
328 and above T_g . All samples showed lower CLTE values below T_g than above T_g . By increasing
329 temperature, the bio-PA tubes offered less resistance against thermal expansion, leading higher
330 CLTE values. The highest CLTE values were clearly observed for PA1010, which is related to
331 the formation of a stronger crystal network that certainly reduces the biopolymer degree of
332 freedom. Similar values were recently reported for compression-molded PA610 parts [48].
333 From the thermal expansion test, T_g values were also obtained, defined as the temperature in
334 which the slope of CLTE changes. As one can observe in the table, these values ranged from
335 40-50°C, following the same trend as the α -relaxation values determined above by DMTA. In
336 general, all bio-PAs presented T_g values close to that of PA6 (~53°C) [47]. Indeed, variations in
337 the aliphatic chain length within the repeating unit are known to have a small effect on T_g of
338 short- and medium-chain polyamides [50].

339 In **Table 2** the values of Vicat softening point and HDT are also listed. These are two important
340 factors when selecting a plastic material for a high-temperature application. In this regard, Vicat
341 reflects the softening degree that would be reached when the bio-PAs are subjected to
342 indentation conditions at a given temperature. In relation to HDT, it determines their upper
343 mechanical use in terms of the temperature limit. In this table, it can be observed that, while
344 PA1010 presented the highest values of both thermomechanical factors, the lowest values were
345 observed for PA610. From the above discussion, these results can be certainly ascribed to the
346 degree of crystallinity observed for the different bio-PAs, showing a good correlation with
347 previous DMTA results. In particular, the here-obtained HDT value for the PA1010 tubes
348 (~60°C) is positively close to that previously reported for injection-molded pieces of PA6
349 (62°C) [51].

350 **3.5. Mechanical properties**

351 **Figure 7** shows the typical tensile stress-strain curves at room temperature for the bio-PA tubes.
352 The mechanical results, in terms of tensile modulus (E), tensile strength at yield (σ_y), and
353 elongation at break (ϵ_b), are summarized in **Table 3**. The mechanical curve of PA610 showed a

354 double yielding while the PA1010 and PA1012 curves displayed a more pronounced ductile
355 behavior. Interestingly, all tensile curves presented strain-hardening phenomenon at large
356 strains. This has been well explained in semi-crystalline polyamides by an induced mechanism
357 of crystals lamellae reorientation process or, in some cases, by a change of both crystal form
358 and size during plastic deformation [52, 53]. The tensile moduli were obtained from the initial
359 linear regions of the curves in the lower strain range, *i.e.* <0.025%. As it was previously
360 observed during DMTA, PA610 showed the highest tensile modulus, *i.e.* 516.8 MPa. This was
361 very similar to that of PA1010, *i.e.* 507.4 MPa, but higher than that of PA1012, *i.e.* 408.6 MPa.
362 However, in relation to tensile strength, the PA1010 tube presented the highest value, *i.e.* ~40
363 MPa, which was approximately 14% and 28% higher than those observed for PA1012 and
364 PA610, respectively. As previously described during the thermomechanical analysis, the
365 enhanced mechanical strength of PA1010 in comparison to the other bio-PA tubes can be
366 ascribed to its higher degree of crystallinity. Furthermore, PA1012 produced the most flexible
367 tubes, showing an elongation-at-break value of approximately 245% due to this bio-PA presents
368 the highest methylene content [54]. Regarding the ductility of the other tubes, PA1010 showed a
369 slightly higher value of elongation at break than PA610, *i.e.* 197% vs. 186%. It is also worthy to
370 note that the here-studied bio-PA tubes presented intermediate elongation-at-break values
371 between those observed for more elastic PA6 (140%) [55] and more ductile PA12 (286%) [56],
372 both processed by injection molding.

373 Finally, in **Table 3** the values of Shore D hardness are also included. One can observe that
374 hardness followed the same trend previously observed in the tensile modulus, having the PA610
375 and PA1010 tubes the highest values. Thus, higher values of hardness can be related to an
376 enhancement of the biopolymer elasticity [57]. However, differences in hardness among the
377 bio-PA tubes were relatively small. In summary, from a mechanical point of view, it can be
378 concluded that PA1010 certainly offers enhanced flexibility with the additional benefit of a
379 relatively high mechanical strength and hardness.

380 **3.6. Water Uptake**

381 Water absorption is one of the most important characteristics of polyamide-based parts for
382 plastics engineering applications. In particular, this phenomenon has been widely studied for
383 polyamides, indicating that water molecules are sorbed only in the amorphous regions by
384 involving two neighboring amide groups in an accessible region [58]. In the first amide, a water
385 molecule is bound by dipole-dipole interactions to the carbonyl groups, *i.e.* hydrogen bonds,
386 while two other water molecules remain loosely bonded in the other amide between the C–O
387 and N–H groups [49]. As it can be observed in **Figure 8**, the immersed bio-PA tubes absorbed
388 different weight amounts of water until these reached a *plateau* after approximately 4 weeks. In
389 particular, water absorption values of 1.93, 1.20, and 0.95 wt.-% were observed for PA610,
390 PA1010, and PA1012, respectively. Therefore, as it has been already established in previous
391 studies concerning polyamides [59], an increase in the CH₂/CONH ratio resulted in a decrease
392 in the water uptake at equilibrium. However, since water is known to be only absorbed by the
393 amorphous phase, crystallinity had a noticeable effect on water uptake too. This explains the
394 significant difference observed between PA610, more amorphous, and the other two bio-PAs. In
395 particular, it is considered that polymer crystallites can hinder translational mobility of water
396 molecules that are sorbed in the amorphous phase [60]. Overall, the water absorption of the
397 here-developed bio-PA tubes was relatively low, in particular when these values are compared
398 to that of conventional PA6 (~8.5 wt.-%) [61]. This encouragingly suggests that their
399 mechanical properties would be scarcely affected by atmospheric humidity.

400 **4. Conclusions**

401 The present study ruled out the differences in the thermal, thermomechanical, and mechanical
402 properties and water uptake of profile-extruded tubes of PA610, PA1010, and PA1012. The
403 obtained data were analyzed and compared in view of their different chemical structures and
404 degrees of crystallinity. It was observed that the CH₂/CONH ratio had a main role in
405 determining the thermal properties, *i.e.* T_g, T_c, and T_m, and water uptake, but it had a lower
406 impact on the thermomechanical and mechanical performance than their crystallinity degree. In
407 particular, it was observed that the PA610 tubes presented a similar thermal performance but

408 lower thermomechanical and mechanical properties than short-chain polyamides, for instance
409 PA6, being relatively rigid at room temperature. Meanwhile, PA1010 interestingly produced
410 semi-crystalline tubes with very balanced physical properties, showing peculiar properties of an
411 engineering thermoplastic. Finally, the PA1012 tubes were much more flexible and these may
412 find applications in the same domain as, for instance, those made of PA12. In general, the
413 PA1010 and PA1012 chemical structures have longer aliphatic segments and lower amide
414 densities than PA610, but these still show higher melting transition temperature than general-
415 purpose plastics such as polyolefins. Therefore, these novel bio-PA tubes can be a good
416 candidate for engineering applications with enhanced sustainable characteristics. **Additionally,**
417 **the effect of chemical agents, fuels, and industrial fluids on the stability and performance of**
418 **these bio-based polyamide tubes would warrant further investigation.**

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425

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TABLES

Table 1. Thermal properties obtained from the differential scanning calorimetry (DSC) and thermogravimetric analysis (TGA) curves in terms of normalized enthalpy of crystallization (ΔH_c), crystallization temperature (T_c), normalized enthalpy of melting (ΔH_m), melting temperature (T_m), amount of crystallinity (X_c), degradation temperature at 5% of mass loss ($T_{5\%}$), degradation temperature (T_{deg}), mass loss at T_{deg} , and residual mass at 650°C for polyamide 610 (PA610), polyamide 1010 (PA1010), and polyamide 1012 (PA1012).

Tube sample	DSC					TGA			
	ΔH_c (J g ⁻¹)	T_c (°C)	ΔH_m (J g ⁻¹)	T_m (°C)	X_c (%)	$T_{5\%}$ (°C)	T_{deg} (°C)	Mass loss (%)	Residual mass (%)
PA610	22.51 ± 1.03	182.6 ± 1.1	15.24 ± 0.85	215.5 ± 1.2	7.8 ± 0.8	331.9 ± 1.5	462.4 ± 1.6	47.3 ± 0.9	0.62 ± 0.06
PA1010	30.77 ± 1.18	176.5 ± 0.9	65.91 ± 0.94	195.4 ± 0.9	27.1 ± 1.2	323.3 ± 1.9	460.7 ± 1.1	47.6 ± 1.3	0.09 ± 0.03
PA1012	25.56 ± 0.96	163.4 ± 0.6	33.59 ± 1.05	183.4 ± 1.1	16.1 ± 0.9	337.6 ± 2.4	463.9 ± 1.3	45.3 ± 1.1	0.21 ± 0.04

Table 2. Thermomechanical properties in terms of the coefficient of linear thermal expansion (CLTE) below and above glass transition temperature (T_g), Vicat softening point, and heat deflection temperature (HDT) for polyamide 610 (PA610), polyamide 1010 (PA1010), and polyamide 1012 (PA1012).

Tube sample	CLTE test			Vicat (°C)	HDT (°C)
	CLTE below T_g ($\mu\text{m}/\text{m}^\circ\text{C}$)	CLTE above T_g ($\mu\text{m}/\text{m}^\circ\text{C}$)	T_g (°C)		
PA610	124.6 ± 1.4	139.8 ± 1.9	49.8 ± 1.2	87.2 ± 1.1	49.2 ± 0.5
PA1010	171.3 ± 1.6	254.6 ± 1.5	45.2 ± 1.3	137.4 ± 1.2	59.9 ± 1.1
PA1012	120.6 ± 1.3	142.2 ± 1.4	42.9 ± 1.4	120.3 ± 1.4	54.5 ± 0.7

Table 3. Mechanical properties in terms of tensile modulus (E), tensile strength at yield (σ_y), elongation at break (ϵ_b), and Shore D hardness for polyamide 610 (PA610), polyamide 1010 (PA1010), and polyamide 1012 (PA1012).

Tube sample	Tensile test			Shore D hardness
	E (MPa)	σ_y (MPa)	ϵ_b (%)	
PA610	516.8 ± 12.1	28.7 ± 0.3	185.6 ± 12.3	64.8 ± 0.8
PA1010	507.4 ± 24.9	39.9 ± 1.3	196.7 ± 11.7	64.2 ± 0.9
PA1012	408.6 ± 15.1	34.3 ± 0.5	245.3 ± 14.4	61.6 ± 1.0

FIGURE CAPTIONS

Figure 1. Chemical structure and bio-based weight content of polyamide 610 (PA610), polyamide 1010 (PA1010), and polyamide 1012 (PA1012).

Figure 2. Schematic representation of the profile extrusion process.

Figure 3. Profile-extruded tubes of polyamide 610 (PA610), polyamide 1010 (PA1010), and polyamide 1012 (PA1012).

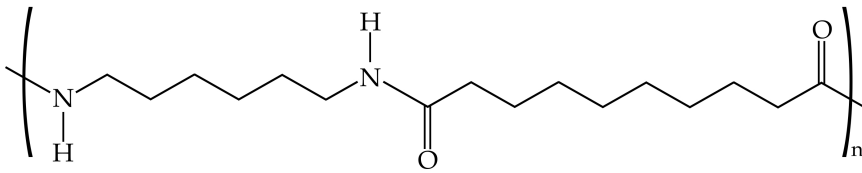
Figure 4. Fourier transform infrared (FTIR) spectra, from bottom to top, of polyamide 610 (PA610), polyamide 1010 (PA1010), and polyamide 1012 (PA1012). Arrows indicate the bands discussed in the text.

Figure 5. Differential scanning calorimetry (DSC) curves of polyamide 610 (PA610), polyamide 1010 (PA1010), and polyamide 1012 (PA1012) for: a) Heating scan; b) Cooling scan.

Figure 6. Dynamic mechanical thermal analysis (DMTA) curves of polyamide 610 (PA610), polyamide 1010 (PA1010), and polyamide 1012 (PA1012) for: a) Storage modulus vs. temperature; b) Damping factor ($\tan \delta$) vs. temperature.

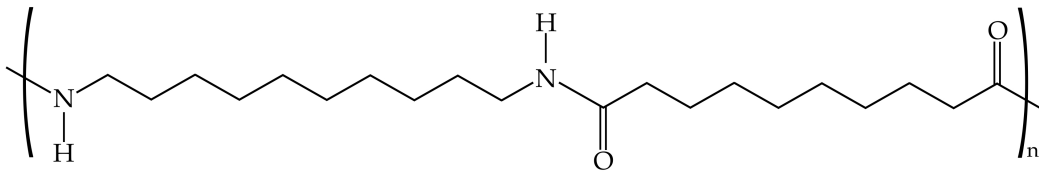
Figure 7. Typical stress-strain curves of polyamide 610 (PA610), polyamide 1010 (PA1010), and polyamide 1012 (PA1012) tubes.

Figure 8. Water absorption of polyamide 610 (PA610), polyamide 1010 (PA1010), and polyamide 1012 (PA1012) tubes.



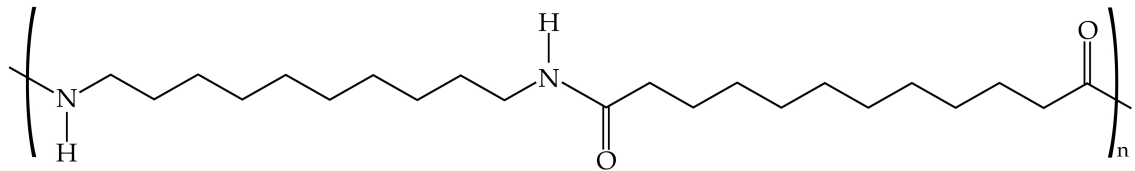
PA610

Based up to 63% on renewable raw materials



PA1010

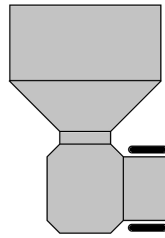
Based up to 100% on renewable raw materials



PA1012

Based from 45 to 100% on renewable raw materials

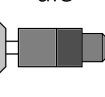
Main hopper



Extruder



Annular die



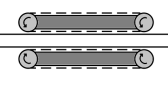
Vacuum sizing chamber



Water cooling bath



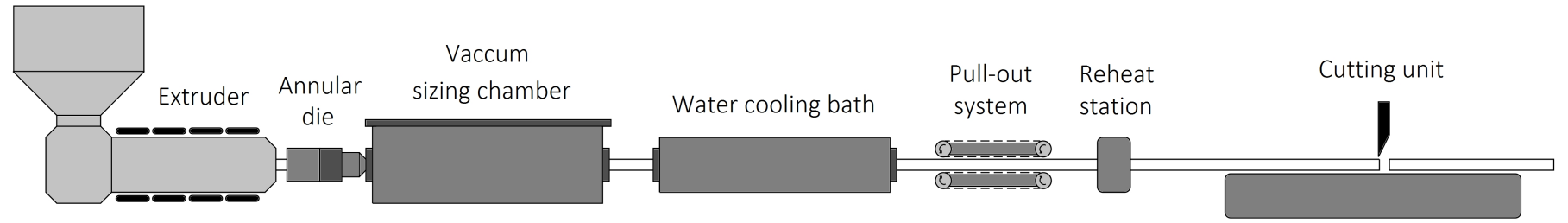
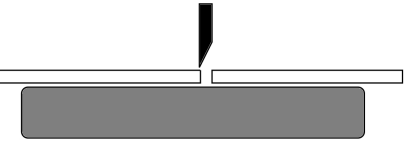
Pull-out system



Reheat station



Cutting unit





PA 610

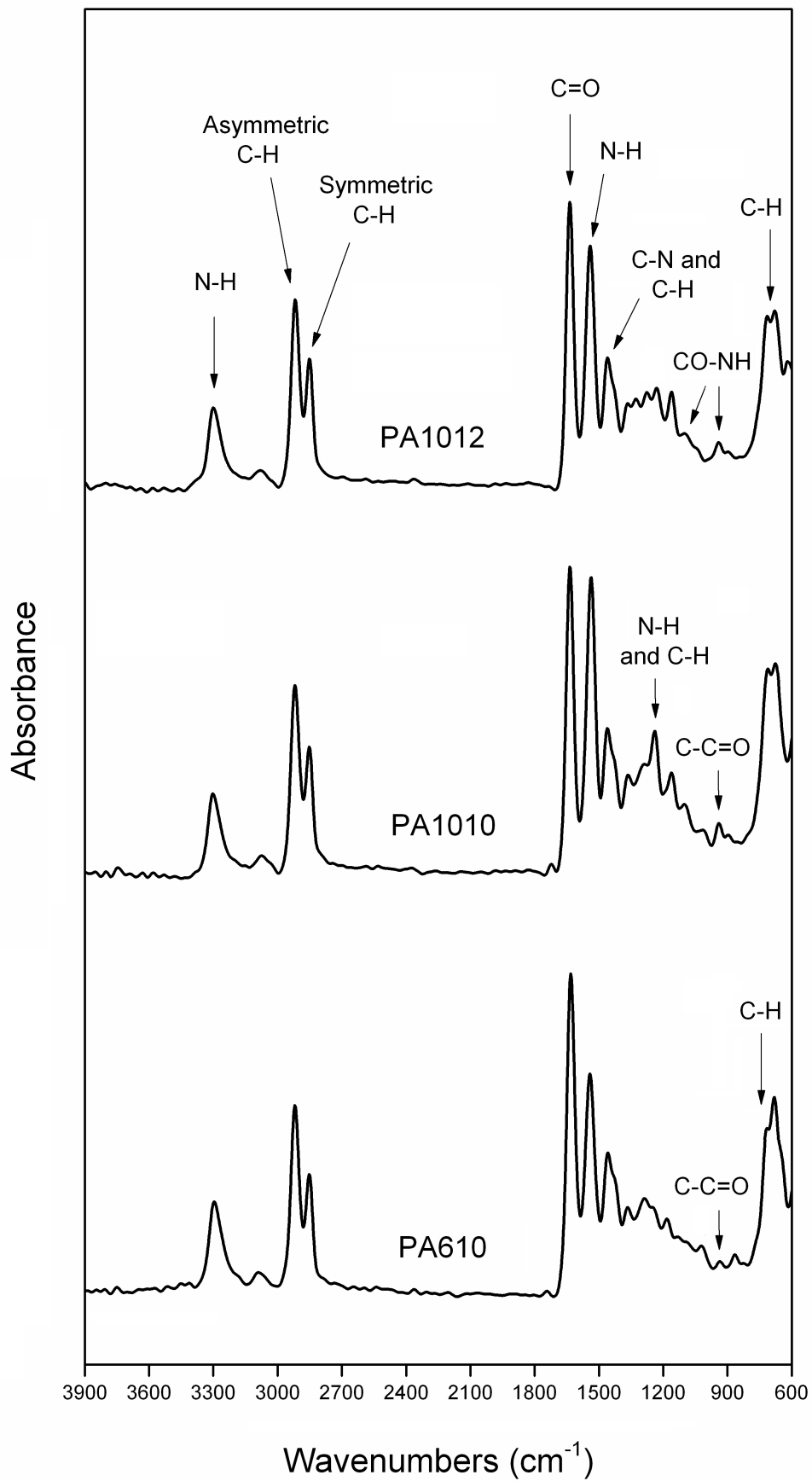


PA 1010

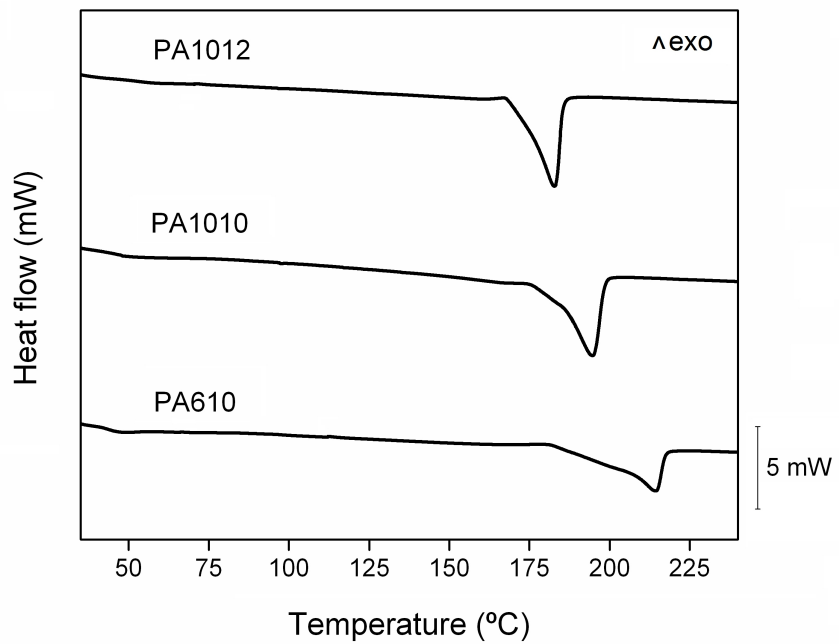


PA 1012

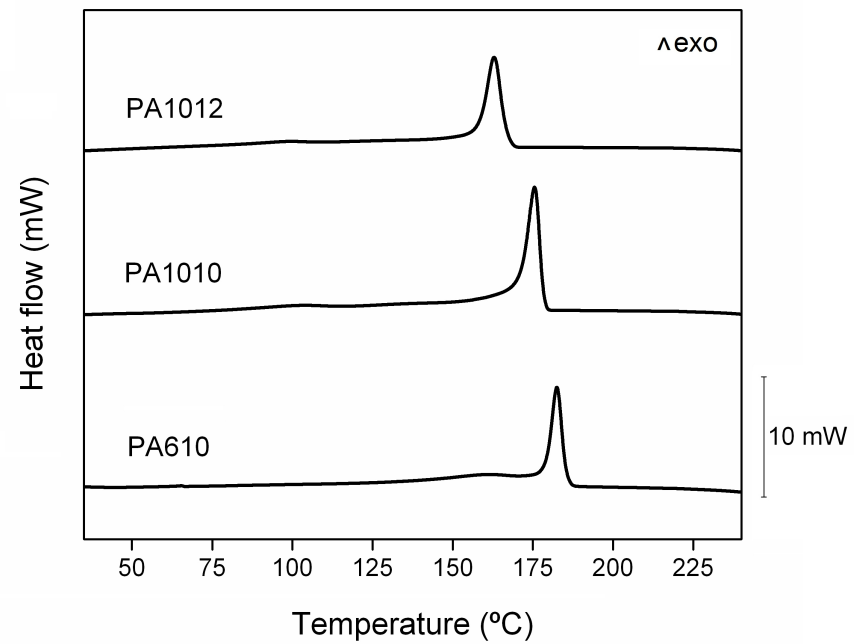
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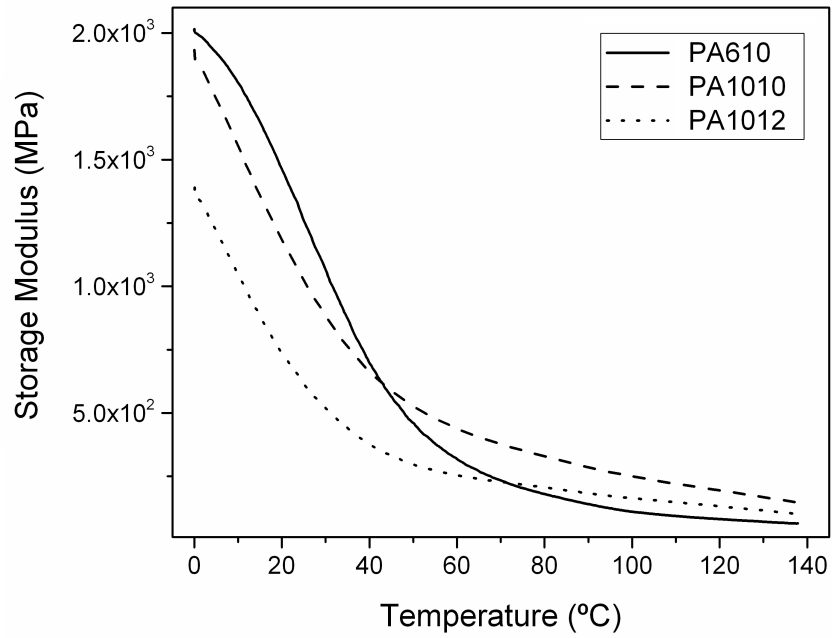
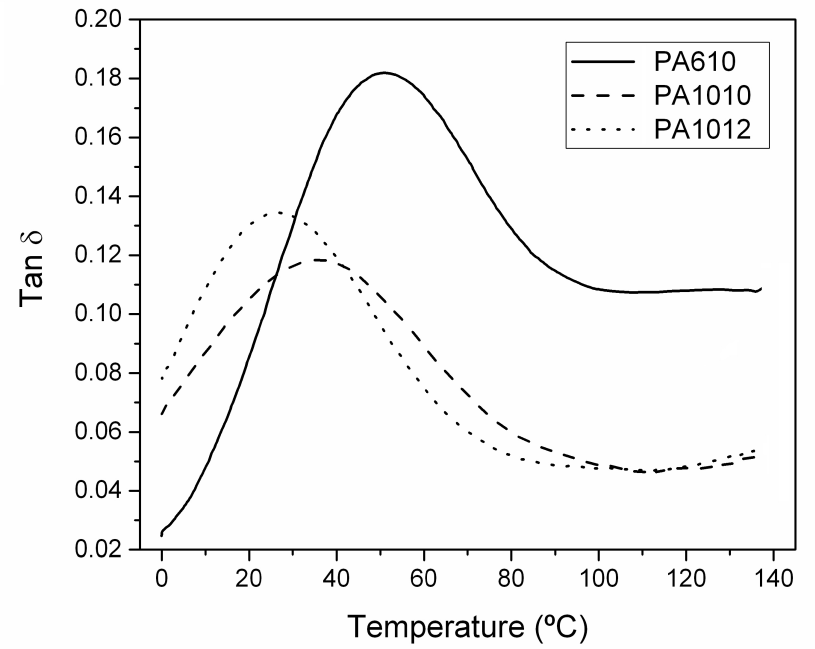


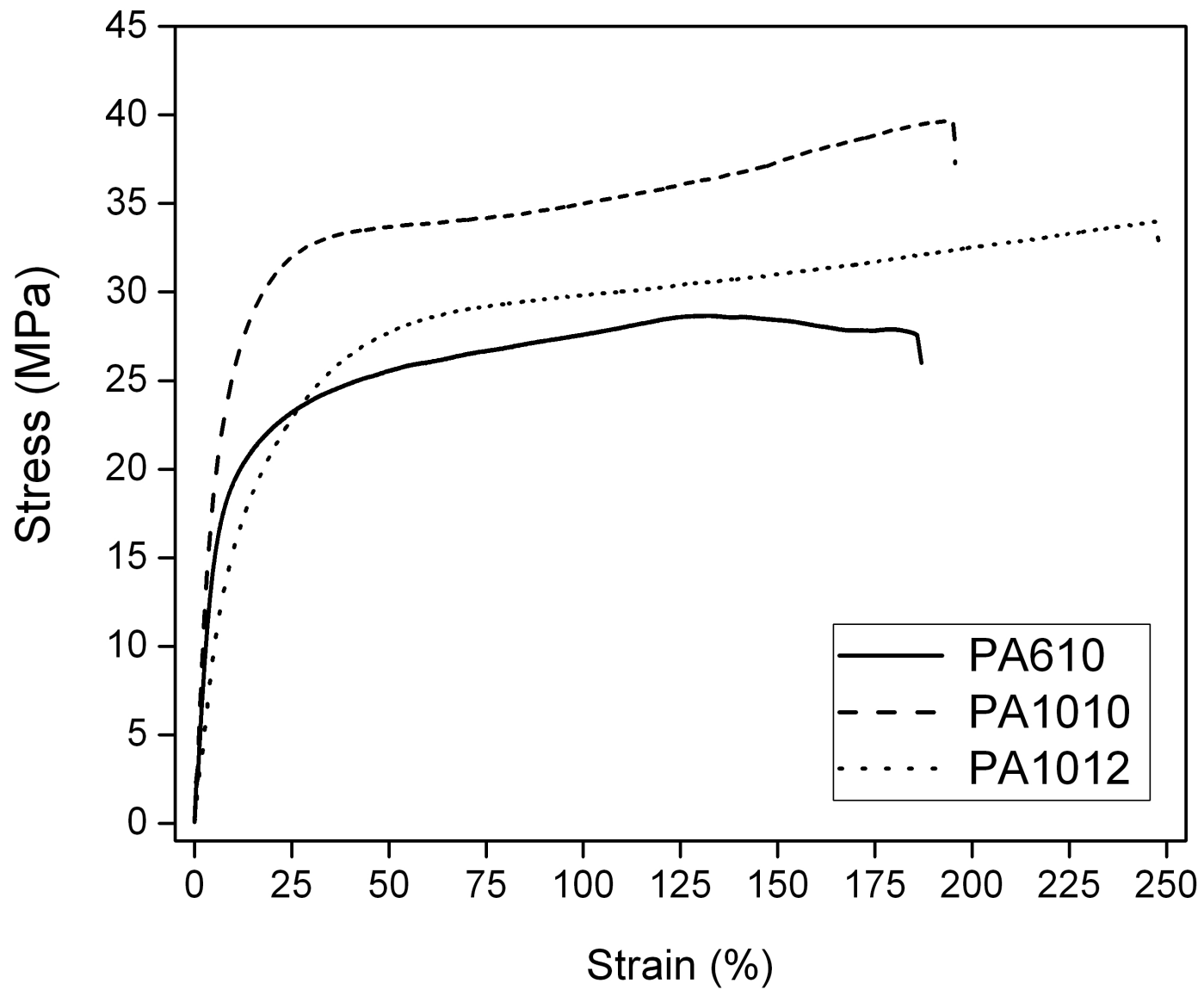
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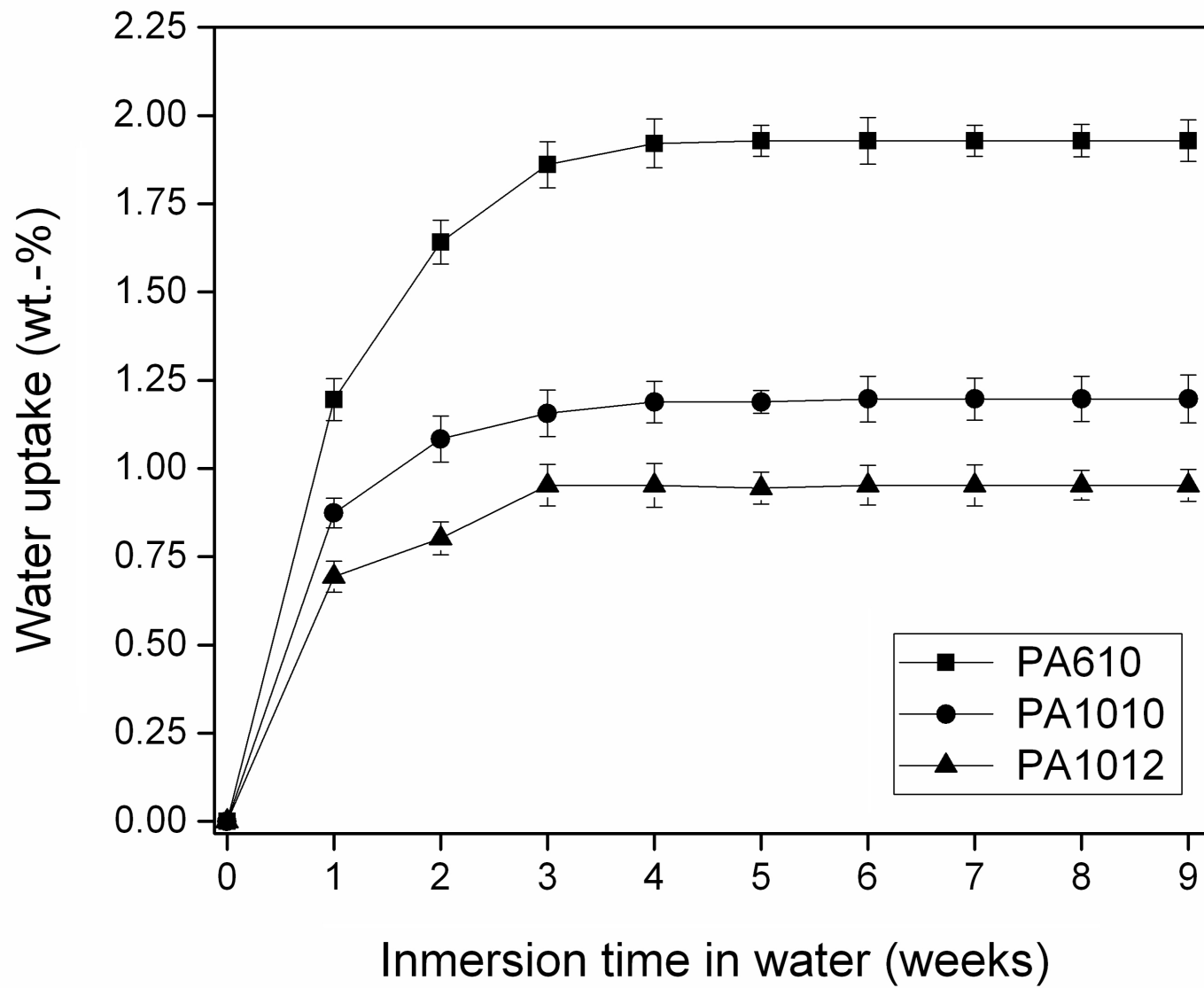


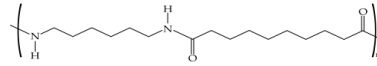
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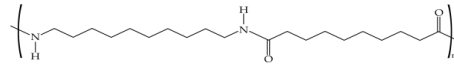
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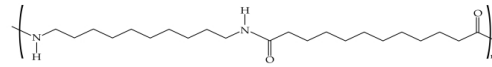




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