

Application of the Monte Carlo method to analyze materials used in flat panel detectors to obtain X-ray spectra

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Abstract. An accurate knowledge of the photon spectra emitted by X-ray tubes in radiodiagnostic is essential to better estimate the imparted dose to patients and to improve the quality image obtained with these devices. In this work, it is proposed the use of a flat panel detector together with a PMMA wedge to estimate the actual X-ray spectrum using the Monte Carlo method and unfolding techniques. The MCNP5 code has been used to model different flat panels (based on indirect and direct methods to produce charge carriers from absorbed X-rays) and to obtain the dose curves and system response functions. Most of the actual flat panel devices use scintillator materials that present K-edge discontinuities in the mass energy-absorption coefficient, which strongly affect the response matrix. In this paper, the applicability of different flat panels for reconstructing X-ray spectra is studied. The effect of the mass energy-absorption coefficient of the scintillator material has been studied on the response matrix and consequently, in the reconstructed spectra. Different unfolding methods are tested to reconstruct the actual X-ray spectrum knowing the dose curve and the response function. It has been concluded that the regularization method Modified Truncated Singular Value Decomposition (MTSVD) is appropriate to unfold X-ray spectra in all the scintillators studied.

KEYWORDS: *Flat Panel, Monte Carlo, unfolding, scintillator materials.*

I. Introduction

Obtaining X-ray spectra in radiodiagnostic units is a complex task mainly due to the high photon flux and the low energy of particles emitted by the tube. To reduce the high fluence reaching the detector, a dispersive or attenuating material is needed. The X-ray spectrum can be estimated using a flat panel detector and an attenuating material.

Flat panels are based on transforming the absorbed X-rays into charge carriers by means of direct or indirect methods. In direct devices, amorphous Selenium (a:Se) is normally used to directly transform photon fluence into current. In indirect devices, a scintillator material absorbs the X-rays and converts them into visible light photons that pass onto a photodiode array. A semiconductor foil is used to convert visible light photons into charge carriers. Normally, amorphous Silicon is preferred as a semiconductor foil to convert visible light photons into charge carriers due to its high rate for Detective Quantum Efficiency (DQE). Although silicon has outstanding electronic properties, it is not a particularly good absorber of X-ray photons. For this reason, X-rays first impinge upon scintillators usually made from either Gadolinium OxySulfide (GOS) or Cesium Iodide. Stopping power, speed and luminosity are the main characteristics to take into account to have a good scintillator material. Stopping power is maximized by maximizing density and atomic number. High density and stopping power are important for reducing the amount of the scintillator material needed (Derenzo and Weber, 2003). Alternative materials like Cadmium Telluride and Mercury Iodide are being studied as they have better stopping power (Hubbell and Seltzer, 2011). Taking into account these considerations, flat panels with different scintillator materials have been analysed.

A PMMA (polymethylmethacrylate) wedge has been used as attenuating material. This wedge is placed between the X-ray focus and the flat panel. When the flat panel is irradiated, a gray-scaled image is obtained. From this image, an absorbed dose curve can be easily obtained. The absorbed dose curve obtained using different scintillator materials can be transformed into tissue equivalent dose multiplying the dose in the first material by the ratio of mass energy absorption coefficients for the second and first material taking into account the photons of interest (always under conditions of secondary charged particle equilibrium).

In this frame, the Monte Carlo code MCNP5 (X-5 Monte Carlo Team, 2003) has been used to simulate the energy absorption in the flat panel and to obtain the dose curve corresponding to certain working conditions of a X-ray tube. The developed MCNP5 model can be used to analyse the behaviour of different scintillators and to determine their response function depending on the X-ray energy. The response function of different materials used in direct and indirect measurements have been determined.

Simulating several monochromatic X-ray beams and calculating the dose curve for each one, the response matrix of the system can be obtained. Knowing the response matrix and the dose curve, the primary X-ray spectrum can be unfolded. However, it has been proved that response matrices characterizing the described problem are ill-posed.

In order to unfold the primary X-ray spectrum, regularization methods can be applied.

Unfolding methods are widely used in different fields of gamma and X-ray spectrometry, environmental radiation, imaging and nuclear data. For instance, the Maximum Entropy Method (MEM) has been successfully used for gamma ray unfolding (Los Arcos J.M, 1996) and for neutron unfolding with the code MAXED (Reginatto et al., 2002). Regarding to nuclear data, the general problem of estimating parameters in nuclear spectroscopy can be undertaken using stochastic numerical Bayesian technique and the reversible-jump Markov-chain Monte-Carlo method (Gulam Razul et al., 2003). Bayesian and Maximum Entropy methods have been used in diagnostic measurements with compact neutron spectrometers (Reginatto et al., 2008). All these methods, partially using the Monte Carlo method, represent some of the new perspectives of spectra and imaging unfolding

In this work, unfolding methods based on the Singular Value Decomposition (SVD) (Golub and Van Loan, 1996) of a response matrix have been used. Specifically, the Truncated Singular Value Decomposition (TSVD), the Modified Truncated Singular Value Decomposition (MTSVD) (Hansen et al. 1992), the Dump Singular Value Decomposition (DSVD) (Hansen et al., 1992), and the Tikhonov method (Hansen, 1999) have been used. These methods have been tested simulating the dose curve for different X-ray spectra extracted from the IPEM 78 Report (Cranley et al., 1997) and verified with experimental measurements.

II. Methodology

1. The Monte Carlo model

The Monte Carlo code MCNP5 (X-5 Monte Carlo Team, 2003) has been used to model an X-ray source, a PMMA wedge and different flat panel detectors including a:Se, CdTe CsI(Tl), GOS and HgI₂.

The theoretical spectra for certain working conditions of the X-ray tube, has been established using the IPEM78 Report Catalogue (Cranley et al., 1997). This actual version uses the XCOM photon cross section library (Berger and Hubbell, 1987) to calculate linear attenuation coefficients of various materials. The unattenuated photon spectra are given for tungsten targets, tube potential from 30 kV to 150 kV, and target angles from 6° to 22°. The ripple value can be changed from 0 to 30%. In this study a Tungsten anode tube has been considered.

The PMMA wedge is placed between the X-ray focus and the flat panel, as it can be seen in Figure 1. A scheme of a generic flat panel model it is shown in Figure 2 with all the materials that conforms a typical flat panel detector. The carbon filter is used to prevent the X-ray penetration the scintillator layer being interfered and absorbed visible light. The scintillator material absorbs the X-rays and converts them into visible light photons that pass onto a photodiode array (fibre optic). The semiconductor foil is used to convert visible light photons into charge carriers.

When the flat panel is irradiated, it registers an absorbed dose gradient due to the attenuation of X-rays produced in the wedge. For certain working conditions (high voltage, filter thickness and current) of the X-ray tube, an absorbed dose curve is obtained.

The absorbed dose curve is directly related to the primary spectrum by means of a Response function. In most applications, the Response function can be approximated by a matrix, which can be obtained using the Monte Carlo method. The photon fluence has been measured in the scintillator layer at 25 different positions along the X axis using a F4MESH tally (X-5 Monte Carlo Team, 2003). Photon fluence can be converted into dose using the

mass energy-absorption coefficient ($\frac{\mu_{en}}{\rho}$) provided by the National Institute of Standards and Technology (NIST) (Hubbell and Seltzer, 2011). The mass energy-absorption coefficients for each material considered in the MCNP5 models are shown in Figure 3.

Common scintillators used in commercial flat panels present a K-edge in the energy range of interest, as it can be seen in Figure 2: GOS (at 50 keV), HgI₂ (at 33.17 and 83.1 keV), CdTe (at 26.7 and 31.8 keV) and CsI (at 33.17 and 35.98 keV), all of them used in indirect methods. On the other hand, a:Se (direct method) does not present any K-edge in the energy range studied (5 to 120 keV). Using this model as a reference, different configurations have been evaluated changing the flat panel configuration. The thickness of scintillator is different in each detector (GOS 0.14 mm (Hamamatsu, 2007), HgI₂ 0.25 mm (Iwanczyk et al., 2001), CdTe 0.2 mm (Izumi et al., 2001) and CsI 0.6 mm (Chabbal et al., 2002)). In the direct flat panel the thickness of a:Se is 1 mm (Izumi et al., 2001).

Each model has been run simulating 50 million particles in order to ensure a relative error in F4MESH lower than 1%. MODE P, E has been activated to follow tracks of photons and electrons. A default cutoff of 1 keV for electrons has been considered.

Figure 4 shows the absorbed dose curves obtained for each case simulating different X-ray spectra varying the high voltage (60, 70, 80, 90 and 100 kV). In all simulations, it has been considered Tungsten X-ray spectra with 12° anode angle and 2 mm thickness of Aluminium filter. All the curves represent absorbed dose in µGy per emitted photon.

As it can be seen the efficiency of the detection produces important variations in the dose curves. Varying the scintillator material there are some bands of energy where absorbed dose curves are clearly separated, while in other intervals of energy they are overlapped.

In the case of CdTe, it can be seen that the absorbed dose corresponding to a 100 kV X-ray spectrum is lower than the corresponding to 90 kV. This fact represents an important disadvantage when primary X-ray spectrum is wanted to be determined using the absorbed dose curves. This point will be discussed in section III.

The MCNP5 model is used to determine different response matrices of the system, one per each flat panel detector. With this aim, different monochromatic beams have been simulated, calculating the absorbed dose curve for each of them. Figure 5 shows the response matrix obtained for each scintillator. In this figure it can be seen the effect of the efficiency on the absorbed dose when the X-ray energy is varied.

The K-edge has an important effect on the response function of the system. Due to the K-edge, the relation between absorbed dose and beam energy is usually not linear. For example, in energies below the GOS K-edge the maximum dose per emitted photon is found at 30 keV. Similar behavior is observed in the other scintillator materials.

Both features (K-edge and efficiency variation) produce an important effect on the reconstruction of the primary spectrum (section III).

2. The unfolding method

The relation between the absorbed dose curve and the primary spectrum can be defined by the Response matrix (R), which can be obtained simulating the response of monochromatic photon beams:

$$R\vec{s} = \vec{m} \quad (1)$$

where \vec{s} is the unknown primary spectrum and \vec{m} is the dose curve registered. This methodology has been applied to the different scintillator materials (a-Se, GOS, CsI(Tl), CdTe and HgI₂) to obtain their Response matrix. Once R is known, the equation (1) theoretically permits to obtain the primary spectrum \vec{s} . But as the determination of this matrix is affected by some errors an approximation $\vec{\tilde{s}}$ to \vec{s} is chosen in such a way that minimizes the 2-

norm of the residual vector $\|R\vec{s} - \vec{m}\|_2$. Singular values of R rapidly decay to 0, being the last singular values very small.

This fact can be seen in Figure 6, where the singular values of different scintillator materials considered in this work are shown. These small singular values make matrix R to be ill conditioned. Condition number of the response matrices are $3.52 \cdot 10^5$ for a-Se, $3.32 \cdot 10^5$ for CdTe, $3.13 \cdot 10^5$ for CsI, $2.99 \cdot 10^5$ for GOS and $1.76 \cdot 10^6$ for HgI₂. The high value of the condition number allows pointing out that these response matrices are ill conditioned.

Due to the fact that R can be considered as rank deficient, there are a large number of solutions for the Least Squares problem $\|R\vec{s} - \vec{m}\|_2$. A fundamental result about rank deficient matrices, which can be derived from the Singular Values Decomposition (SVD) of R, is that closest rank-k approximation R_k to R is obtained by truncating the SVD expansion at k, removing the parts of the solution corresponding to the smallest singular values (Golub and Van Loan, 1996). The Truncated SVD (TSVD) and the Modified TSVD (MTSVD) regularization methods are based on this observation in that one solves the problems:

$$\min \|\vec{s}\|_2 \text{ subject to } \min \|R_k \vec{s} - \vec{m}\|_2 \quad (2)$$

$$\min \|L\vec{s}\|_2 \text{ subject to } \min \|R_k \vec{s} - \vec{m}\|_2 \quad (3)$$

respectively.

In the MTSVD method, equation 3, the 2-norm $\|\vec{s}\|_2$ is replaced by the seminorm $\|L\vec{s}\|_2$, where L is a discrete approximation to the p'th derivative operator (Hansen et al., 1992).

Finally, Tikhonov regularization method (Hansen, 1999) is based on a modification of the Fredholm integral equation of the first kind (a classical example of an ill-posed problem) that is intended to stabilize its solution. This is achieved by constructing the following functional:

$$f(x) = \|R\vec{s} - \vec{m}\|_2^2 + \lambda \|L\vec{s}\|_2 \quad (4)$$

The idea is to define the regularized solution \vec{s} as the minimizer of the following weighted combination of the residual norm and the side constraint

$$\vec{s} = \operatorname{argmin} \left\{ \|R\vec{s} - \vec{m}\|_2^2 + \lambda^2 \|L\vec{s}\|_2^2 \right\} \quad (5)$$

where the regularization parameter λ , controls the weight given to minimization of the side constraint relative to minimization of the residual norm. L takes different forms in accordance with the order of regularization. Different L operators can be used (I, L₁ or L₂). In this paper it has been chosen the second order Tikhonov regularization, L₂.

$$\mathbf{L}_1 = \begin{bmatrix} 1 & -1 & & & & & & & \\ & 1 & -1 & & & & & & \\ & & 1 & \ddots & & & & & \\ & & & \ddots & \ddots & & & & \\ & & & & \ddots & -1 & & & \\ & & & & & 1 & -1 & & \\ & & & & & & & 1 & \\ & & & & & & & & 1 \end{bmatrix}$$

matrix and dose curve for each unfolding method. As it can be seen, the optimal value of the truncation parameter is almost constant in the voltage interval considered for each unfolding method. For TSVD method $k=4$ has been used in all the cases except for the GOS ($k=5$). For MTSVD has been considered $k=3$ in all the cases. More differences between each material are found in the Tikhonov method (λ a:Se = 8.50×10^{-8} , λ CdTe = 4.40×10^{-7} , λ CsI, GOS, HgI₂ = 2.40×10^{-7}).

III. Results and Discussion

The optimal choice of the truncation parameter, k or λ , contributes to obtain a best fit of unfolded spectrum respect to the theoretical primary beam spectrum. When k or λ is greater than the value given by the L-curve corner, fluctuations and noise increase in the unfolded spectrum. On the other hand, when k or λ is lower, unfolded spectrum is over smoothed, losing information.

In Figure 9, it is shown a comparison between theoretical 100 kV spectrum and unfolded spectra obtained applying the MTSVD method for different regularization parameter k . As it has been said, solution is highly affected by the choice of k . Furthermore, the characteristic lines of tungsten are not present in the unfolded spectra. An analogous analysis can be done in the case of Tikhonov unfolding.

Once the k parameter has been fixed for each unfolding method and each response matrix, the methodology has been tested for different tube working conditions varying the peak high voltage.

Figures 10 to 16 show comparisons between unfolded and IPEM78 theoretical spectra for 70 kV and different flat panel configurations. TSVD, MTSVD, DSVD and Tikhonov methods have been applied to reconstruct primary spectra.

In the case of a:Se, MTSVD ($k=3$) successfully fits theoretical spectra. Figure 10 shows a comparison of unfolded spectra (using the regularization methods MTSVD and Tikhonov). In all cases, a smooth solution is obtained thanks to the derivative operator L_2 . Bremsstrahlung distribution obtained with MSTVD adequately reproduces the theoretical spectra. However, the maximum of the Bremsstrahlung continuous is reached 10 keV above the maximum of the theoretical spectra. The most important discrepancies are found in the energy range defined between 40 and 70 keV. Regarding to Tikhonov regularization ($\lambda=8.50 \times 10^{-8}$), smooth spectra are obtained, but Bremsstrahlung continuous is shifted about 10 keV to the low energy range.

When L_2 operator is not considered, important discrepancies appear (fluctuations and distortions of the spectra). This effect can be observed in Figure 11. In this case, TSVD, DSVD and Tikhonov ($L=I$) have been applied to unfold spectra of 70 and 100 kV. Reconstruction obtained with TSVD method shows slight fluctuations in the whole energy interval. TSVD unfolded spectrum present more important discrepancies when high voltage is reduced. In fact, only an accurate spectrum is obtained for 100 kV. DSVD method does not offer acceptable results in any case.

In general, using TSVD, DSVD and Tikhonov ($L=I$) important fluctuations and noise appear in unfolded spectra. Furthermore, solution is distorted and shifted to the high energy range. In the case of DSVD and Tikhonov ($L=I$), the regularization methods are not able to adequately determine the maximum energy of the Bremsstrahlung continuous. This fact is more evident in the 70 kV spectrum (in both methods, the maximum energy of the distribution reaches 100 keV). In any case, characteristic lines are not reproduced.

As a conclusion, it can be said that the derivative operator, L_2 , is necessary to smooth the spectra in order to obtain an acceptable estimation of the primary spectra.

Figure 12 shows the unfolded spectra obtained when CdTe response matrix is considered. It can be observed the same general trends explained for a:Se. It is needed the derivative operator L_2 to obtain a smooth and adequate solution. The weak point of choosing CdTe to reconstruct spectra is its poor behaviour for voltages greater than 90 kV. In Figure 12 it can be clearly seen that the worse reconstructions are found for 100 kV, independently of the unfold method used. This effect can be attributed to the reduction of detection efficiency for energies greater than

90 keV. Unfolded spectra obtained with TSVD and Tikhonov ($L=I$) do not fit theoretical spectra for any tested voltage (70 up to 100 kV), as it can be seen in Figure 13. It is the same behaviour than with a:Se.

In Figures 14, 15 and 16, it is shown the unfolded spectra obtained applying the MTSVD and Tikhonov (L_2) regularization methods to CsI, GOS and HgI₂ matrices, respectively. The behaviour of solutions is quite similar in all cases. MTSVD unfolded spectra are shifted to the low energy range, and Tikhonov spectra to high energies. K-edge appearing at different energies do not produce any particular effect on the reconstructed spectra. It can be stated that K-edge of scintillator does not have a relative importance to cause the ill-posed problem.

From all these results, some points should be highlighted: K-edge of different response matrices do not alter the ill-posed condition of the problem and do not affect the quality of the unfolded spectrum. The condition number of the response matrix does not depend on K-edge. It has been proved that the response matrix of all material analysed have a similar condition number (about 105), also with similar singular value decomposition. However, the efficiency of some scintillators is gradually reduced for energies up to 100 keV, for example CdTe. In this case, regularization methods such as MSTVD or Tikhonov do not adequately unfold spectra. On the other hand, it is necessary to consider a derivative operator (L_2) to obtain a smooth unfolded spectrum. In general trends, from the mathematical point of view, it seems that the scintillator material does not represent a relevant aspect to unfold primary spectra. However, choosing the adequate regularization method is very important to obtain acceptable unfolded primary spectra.

IV. Conclusions

The applicability of the system PMMA wedge-Flat panel to reconstruct primary X-ray spectra has been analysed. It has been stated the suitability of the MTSVD and Tikhonov regularization methods to unfold X-ray spectra in the considered energy range.

A MCNP5 model to simulate the actual acquisition process has been developed. Different materials used in commercial flat panels have been tested using this model. The response matrix corresponding to each scintillator has been obtained simulating several monoenergetic photon beams. The response matrices obtained have a large condition number, pointing out an ill-posed problem. Two features can, a priori, affect the quality of the solution: variation of efficiency depending on energy and the K-edge of the scintillator. To study these hypotheses, five response matrices of different scintillators have been analysed and used to unfold primary X-ray spectra in the radiodiagnostic range.

Regularization methods such as MTSVD and Tikhonov are able to unfold primary spectra when a derivative operator is used to smooth the solution. TSVD, DSVD and Tikhonov (using L as identity) do not offer good results in any case. In any case, characteristic lines are not properly unfolded.

The K-edge does not have a relevant effect in the unfolded spectra. However, the variation of efficiency strongly affects the quality of the unfolded spectrum.

From the point of view of X-ray unfolding, it has been proved that CdTe does not allow obtaining acceptable results for voltages greater than 90 kV.

It is recommended the use of the regularization MTSVD method for any kind of scintillator used.

The effect of the K-edge is negligible during the unfolding process.

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Table 1: Regularization parameters